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- 1 Advancing dosimetry for Dating Environmental Materials: Development of an ultra-sensitive beta
- 2 dosimeter system and potential for beta autoradiography
- 3 Martin, L.^{1,2,*}, Sanderson, D.¹, Paling, S.³, Cresswell, A.¹, Murphy, S.¹
- 4 ¹ Scottish Universities Environmental Research Centre, Glasgow, United Kingdom
- 5 ² Royal Society Newton International Fellow
- 6 ³ Boulby Underground Laboratory, Saltburn-by-the-Sea, United Kingdom
- 7 *Presenting Author: loic.martin@glasgow.ac.uk
- 8

9 Abstract

10 Beta Dose Rate heterogeneity is a recognized source of uncertainty when applying luminescence dating to 11 heterogeneous samples, such as coarse crystalline rocks and clast-rich sediments. Simulations have shown that 12 a combination of a heterogeneous distribution of minerals and radioactive elements can lead to complex dose 13 distributions, overdispersion and potentially to bias in equivalent dose determinations. However setting realistic 14 conditions for such simulations remains difficult, and there are at present only a few experimental validation cases 15 for such simulated systems. Project ADDEM is investigating means of linking Monte Carlo simulations of dose rate 16 to specific minerals with direct observations using high sensitivity phosphor plates and laser scanning imaging 17 systems in combination with phase mapping. To overcome some of the limitations of autoradiographic imaging of 18 low level beta dose distributions work has been undertaken using Landauer alumina OSL phosphor screens in 19 combination with a laser scanning system developed at the Scottish Universities Environmental Research Centre 20 (SUERC). Preliminary excitation spectra, emission band characterisation and time resolved measurements were 21 undertaken, confirming the potential to recording low doses using asynchronous stimulation at 635 nm coupled 22 with blue band detection. Taking advantage of the slow decay of the luminescence signal the scanning equipment 23 has been configured for pulsed stimulation and asynchronous detection to maximise signal to background ratios. 24 Exploratory work was calibrated using a ⁶⁰Co facility capable of calibrating doses in the µGy to mGy range. A series 25 of powdered granulite/basalt mixtures of known mean activity and dose rate (Dr) have also been used to calibrate 26 the phosphor screens. To reduce background levels during autoradiographic signal accumulation rock slices are 27 being exposed in the Zeplin shield of the STFC Boulby Underground Laboratory, in an environment which is 28 essentially free from cosmic ray muon background. 29 Simulations have been conducted providing preliminary deconvolution parameters in order to either reconstruct 30 the beta dose rate (β Dr) distribution received by the grains in the sample, or retrieve the radioactive element 31 distributions in the minerals of the sample, providing the data required for representative simulations of β Dr. 32 This paper outlines the spectroscopy and sensitivity verification of the autoradiography system, confirming its

- prospects for measuring spatially resolved β Dr distributions with single pixel lower detection limit of 130 μ Gy and spatial resolution of 150 μ m. Prospects are outlined.
- 35
- 36 Keywords: beta dose rate; Alumina OSL dosimeter; mapping; simulation; pulsed OSL.
- 37

38 1. Introduction

Beta dose rate (β Dr) heterogeneity in unconsolidated sediments and rocks is a known source of overdispersion in luminescence dating (Nathan et al., 2003). As aliquot sizes have been reduced in response to improved sensitivity in dating analyses it has been highlighted as one of the main sources of overdispersion of equivalent doses, in particular when single grain analyses are involved (Duller et al., 1999). However, β Dr distribution is still difficult to characterize because of the low dose rates of natural samples, the sub-millimetre variations of beta dose rates, and uncertainties associated with in-grain luminescence sensitivity distributions. 45 Several attempts have been made to map β Dr distributions using phosphor dosimeters (Rufer and 46 Preusser, 2009; Guérin et al., 2012b; Smedley et al., 2020), measurements of β radiation emitting elements 47 (Jankowski and Jacobs, 2018) or semi-conductor detector cluster Timepix (Romanyukha et al., 2017). Despite the 48 new insights that these studies have brought to β Dr heterogeneity, quantification of results remains difficult either 49 because of the lack of a suitable calibration method, of low dosimeter sensitivity leading to large uncertainties, or 50 limitations to spatial resolution on the scale of individual grains and subgrains.

51 Different approaches aiming to model the beta dose rate distribution instead of measuring it have also 52 been developed. Dose point kernel modelling coupled to 3D phase mapping (Plachy and Sutton, 1982) and Monte 53 Carlo modelling (Nathan et al., 2003; Mayya et al.; 2006, Guérin et al.; 2012a; Martin et al., 2015; Martin et al., 54 2018) have both shown the capability of modelling beta dose rate distributions of heterogeneous samples. However, 55 the reliability of these methods strongly depends on the exactness of the input data of the model. Therefore they 56 require extensive characterization of samples with a sub-millimetre resolution to be able to resolve the beta dose 57 rate heterogeneity, which in turn is limited by the accuracy and resolution of available methods. In addition, only a 58 few experimental validations of the results of these models for luminescence dating samples have been carried out 59 (Nathan et al., 2003; Cunningham et al., 2012).

60 The characterization of beta dose rate heterogeneity, in term of intensity and spatial distribution, requires 61 high sensitivity (sub-mGy level), high resolution (sub-mm) and a calibration method adapted to imaging. As a first 62 part of the project ADDEM (Advancing dosimetry for Dating Environmental Materials) we investigated carbon 63 doped alumina (Al₂O₃:C) OSL dosimeter films developed by Landauer Ltd (Glenwood, IL, USA) (Endo et al., 2012) 64 for implementing an ultra-sensitive β autoradiography system suitable for heterogeneous natural samples used in 65 luminescence dating. The properties of this phosphor dosimeter in terms of excitation, decay time and dose 66 response have been investigated for the first part of project ADDEM. These data have been used to improve the 67 signal to noise ratio in a high-resolution laser scanning OSL system. Initial results of Monte Carlo models to 68 calibrate the phosphor response and deconvolve the image to determine the ß Dr distribution in the sample are 69 presented.

70 2. Sample and methodology

71 **2.1 Dosimeter film and samples**

72 Al₂O₃:C is known to be a highly efficient dosimeter for both Optically stimulated Luminescence (OSL) and Thermoluminescence (TL) (McKeever et al., 1999). Although it is well studied in the context of dosimetry for 73 74 radiation workers, involving Gy level dose or higher (McKeever et al., 1999), fewer studies have considered the 75 sensitivity and dose response curve at mGy and sub-mGy levels (Markey et al., 1995; McKeever and Akselrod, 76 1999; Kalchgruber et al., 2003). The film used for this study is a 47 µm thick deposit of Al₂O₃:C grains in a polyester 77 binder on a 75 µm thick polyester substrate (Fig. 1). The grains have been measured to be about 15 µm in diameter. 78 The substrate is translucid, allowing luminescence emission in all direction. This film was provided to Scottish 79 Universities Environmental Research Centre (SUERC) as a 22.5 cm by 28 cm sheet that can be cut to the required 80 sizes.

81 Figure 1

In addition to the high sensitivity of this material a linear dose response curve- is expected from mGy to Gy level. Its linearity for sub-mGy level is investigated during this study. The small thickness of the film will benefit the imaging resolution, as it limits the spreading of beta radiation in the thickness of the sensitive layer, decreasing the need for deconvolution corrections for dose mapping. It is reusable, which combined with the possibility of cutting it to sizes suitable for particular samples makes it practical for regular measurement. The dimensions of the pieces of film cut for this study ranged from 5 mm to 20 mm.

A series of powders of homogenised granulite and of basalt have been prepared at SUERC for use as a
 new generation of internal dose rate standards (Sanderson personal communication). Here the end members and

- 90 mixtures of 50 % and 25 % 75 % in mass of each have been used, their contents of radioactive elements have
- 91 been measured by high resolution gamma spectrometry and ICPMS analysis and will be reported elsewhere.
- 92 Meanwhile table 1 gives the working concentrations of the materials used here. These powders were used for an
- 93 experiment of exposure of the Al₂O₃:C film to beta dose rate. An inert powder of sodium carbonate Na₂CO₃ was
- 94 used for blank measurements.
- 95 Table 1

96 2.2 Equipment and method

97 2.2.1 Excitation spectrometer

98 Excitation spectra were recorded using the SUERC spectrometer originally developed for research on 99 detection of irradiated foods (Sanderson, 1991), and later applied to studies of feldspars (Clark, 1992; Clark and 100 Sanderson, 1994). Fig. 2 shows a simplified schematic diagram. It uses a 300 W Xenon Cermax lamp as a light 101 source, which incorporates a parabolic reflector resulting in high intensity forward beams. A stepper motor driven 102 Applied Photophysics monochromator, with adjustable slit widths and order sorting filters on entrance and exit for 103 wavelength selection, followed by collimating optics leading to the sample chamber is used. Samples are 104 illuminated on an inclined samples stage. Luminescence is detected using filtered single photon counting tubes 105 (Electron Tubes 9883 QA/QB) with fast amplifier discriminators and recorded using a 2000 channel Ortec 106 multichannel scalar (MCS) system. For this work the PMT was filtered with BG1/BG3 filters to record the near UV 107 and blue emission of the alumina films, with the stimulation light filtered by a 470 nm long pass filter. The 108 luminescence signals from a 5x5 mm piece of Al₂O₃:C film, beta irradiated with 100 Gy, was recorded while the 109 monochromator wavelength was decremented from 750 nm to 480 nm. In earlier work a pyroelectric radiometer 110 was used to normalise the measured spectra (Clark, 1992, Clark and Sanderson, 1994). Here intensity measured 111 were normalized using the theoretical intensity spectra of the Xenon lamp. The excitation spectrum obtained is 112 presented in Fig. 6.

113 Figure 2

114 2.2.2 Time resolved OSL reader

115 Time resolved OSL measurements were made here using diode stimulation, based on pulse generators 116 and transistor driven systems developed in earlier work (Sanderson & Clark, 1994). A schematic of the system 117 used here is shown in (Fig. 3). A TTL oscillator module capable of generating 5 V diode pulses with adjustable 118 pulse widths (down to 1 µs) and delays between pulses ranging from 12 µs to 1.2 s was used. For this study 119 clusters of 3 LEDs of 635 nm wavelength were used to stimulate the sample. The OSL signal is collected by a 120 photomultiplier with a 3 mm BG3 filter. While not completely eliminating the within-pulse background from the 635 121 nm diodes, this detection band filtration is enough to protect the photomultiplier while allowing more than 80 % of 122 the luminescence signals from the Al₂O₃:C film to pass. While the use of a more efficient wavelength in the 525 nm 123 to 550 nm range would have produced more luminescence per unit of time, this would have been too close to the 124 main emission band of Al₂O₃:C and therefore requiring a larger thickness of BG3 filter (12 mm minimum) in order 125 to protect the photomultiplier. This would significantly decrease the luminescence signal passing through the filter, 126 at the point that the signal measured is not significantly more than with the 635 nm stimulation and 3 mm BG3 filter. 127 In addition, for the laser scanning system that is described below, the use of 525 nm to 550 nm wavelength laser 128 increases the risk of damaging the photomultiplier in case of a direct beam reflection. It also prevents the possibility 129 of doing successive imagings of the same irradiation, as the bleaching of luminescence signal by the laser would 130 also be significantly faster than with the 635 nm laser stimulation.

The detection during a defined time window was synchronised by starting MCS capture at the beginning of each stimulation pulse using the TTL drive signal. The counts from each stimulation pulse were then registered in the MCS and used to define the luminescence relaxation decay times. Similar systems were used by Markey et al. (1995) or Yukihara and McKeever (2006) to perform time resolved analysis of Al₂O₃:C. The time resolved analysis of a 5x5 mm piece of Al_2O_3 :C film irradiated with 100 Gy is presented on Fig.7, recorded using 130ms

 $136 \qquad \text{stimulation pulses with a 1500 ms delay, over about 20 min.}$

137 Figure 3

138

2.2.3 Laser scanning imaging OSL reader

139 The imaging OSL readers from Sanderson et al. (2001) (Fig. 4) were designed to map the luminescence 140 signal from a sample pixel by pixel. The sample is placed on a support on a plate moved by two perpendicular 141 stepper motor axes (X and Y axis). Based on the review of the excitation and time resolved spectrometry of the 142 alumina film one of these systems has been configured with a 635 nm 5 mW Acculase model laser from Global 143 Laser LTD (Abertillery, UK), and detection band photon counting with BG3 filtration. The laser has a beam size at 144 nearest focus of < 50 µm, bringing the beam from a working distance of 10 cm at a 45° angle results in a spot size 145 <100 µm at this stage of the work. The luminescence is recorded by a photomultiplier above the sample, then the 146 plate moves one step for the next measurement. Setting the system up in this way allows the luminescence signal 147 measured from the sample during the decay after stimulation to be optimised while using a pulsed OSL (pOSL) 148 protocol (Markey et al., 1995; McKeever and Akselrod, 1999, Yukihara and McKeever, 2006). The stimulation 149 sequence is composed of successive stimulation pulses followed by measurements of the luminescence signal 150 during its decay. This protocol was chosen in consideration of the properties of the OSL film determined by the 151 previous analysis (see Results part). The measurements on each point are preceded by several dark count 152 measurements. This succession of dark count measurement is used to determine if a luminescence or 153 phosphorescence signal persists from the previous measurement, by comparison of dark count prior to the start of 154 any measurement and by checking if the signal is decaying. No significant signal remaining from the previous point 155 of measurement was observed in this study. The average dark count was calculated as the mean value over 156 successive measurements.

157 Figure 4

158 2.2.4 Irradiation of dosimeter films

159 In order to estimate the signal from sub-mGy doses and to test the linearity of the film response to dose, 160 a piece of 10x15 mm film was irradiated using a 60 Co gamma source with doses from 139 ± 8 to 739 ± 33 mGy. 161 The piece of film was covered a 3 mm of aluminium sheet during gamma irradiation in order to generate charge 162 particle equilibrium. Before each irradiation, the sample was bleached under white light, through a GG 495 nm long 163 pass filter to cut UV wavelength and reduce charge transfer from deep traps during bleaching. It was then scanned 164 with the laser scanning OSL reader using 500 µm steps and a sequence of 300 ms of dark count measurement 165 followed by 100 repetitions of the cycle "60 ms of laser stimulation - 30 ms of measurement during the 166 luminescence signal decay". The resulting images can be observed in Fig. 8, while the calibration curve resulting 167 from the integrated signals over the image is presented in Fig. 9. Limits of detection and of quantification resulting 168 from these results are illustrated in Fig. 10.

169 2x2 cm pieces of dosimeter film were exposed to powdered samples of granulite-basalt mixtures (table 1) 170 and pure sodium carbonate, the last one being used as blank. They were bagged in pairs in dark polyethylene 75 171 µm thick bags, which is enough to shield from the alpha particles and protect the phosphor from light exposure, 172 with the sensitive parts turned outwards. The bagged dosimeter films were placed in the centre of 5 cm diameter 173 by 1.8 cm high cylindrical plastic containers filled by the powder samples, according to the geometry presented in 174 Fig. 5a. This ensures that the bagged films are surrounded by at least 5 mm of powder on every side, which is 175 enough to create an infinite matrix condition in regard of the beta dose rate. The containers were placed in a 10 176 cm thick lead castle with a 1.5 mm inner layer of copper (Fig. 5b), for shielding from the environmental X-rays and 177 gamma radiation, as well as from the soft cosmic component. The exposure time was about 1 year and 4 months. 178 The dose rates were estimated using the radioactive element contents from table 1, and the conversion factors 179 from Cresswell et al. (2018). The beta attenuation factors by the dosimeter and protective layer were calculated

180 from modelling, as well as the gamma dose rate contribution (table 2). Each calculated dose was adjusted 181 considering the exact time of exposure within an uncertainty of one day. They were read with the laser scanning 182 OSL reader using 250 µm steps and a sequence of 300 ms of dark count measurement followed by 100 repetitions 183 of the cycle "60 ms of laser stimulation - 30 ms of measurement during the luminescence signal decay". They were 184 then bleached for 48 h under non-UV white light and scanned again to measure the background signal. The results 185 of counts per pixel compared to the estimated dose are plotted on Fig. 11a. Equivalent gamma dose for the 186 measured luminescence signal were obtained by irradiating the same dosimeter film with a calibrated ⁶⁰Co gamma 187 source: each film was exposed to a dose of 900 µGy and their luminescence signal was measured again using 188 the same protocol; the ratios of powder exposure signal to the gamma source exposure signal were used to 189 calculate the gamma doses equivalent to the powder exposure signal. These equivalent doses are compared with 190 the calculated exposure dose on Fig. 11b.

191 2.3 Modelling

192 Monte Carlo simulations of the irradiation of the film were conducted to calculate the attenuation during 193 exposure of the sample and to investigate the correspondence between the mapped OSL signals and the Dr 194 distribution in the sample. There were conducted using the Geant4 toolkit (Agostinelli et al., 2003; Allison et al., 195 2016), that already have been successfully used in the context of luminescence dating (Guérin et al.; 2012a; Martin 196 et al., 2015; Martin et al., 2018). The simulation code allows stacking different types of slices: radioactive mineral, 197 phosphor, phosphor substrate, phosphor cover, absorber. The composition and density of each type can be 198 adjusted. The phosphor layer is divided into pixels of adjustable size, each pixel records the dose received from 199 the radioactive mineral layer. The distribution of radioactivity in this layer can be uniform or follow certain patterns 200 such as a rectangle, a dot or a sphere. The spectra for the beta and gamma emissions of ⁴⁰K, of U-series and of 201 Th-series were constructed using the Geant4 database, whose data comes from the Evaluated Nuclear Structure 202 Data File (ENSDF) which is maintained by the National Nuclear Data Center, Brookhaven National Laboratory 203 (USA). It is noted that emission spectra in other nuclear databases vary from the ENSDF used here, as recently 204 discussed by Cresswell et al. (2019), but these differences have not currently been considered. The PENELOPE 205 code for low-energy particle physics (Baró et al., 1995; Ivanchenko et al., 2011) was used for calculating the beta 206 interactions through matter.

Simulations of the exposure of two OSL films protected by a 75 µm thick dark plastic bag to granulite powder (composition given in table 1, density 2.0 g.cm⁻³) were conducted (Fig. 5a). The resulting beta attenuation coefficients are presented in Table 2. The gamma dose contribution to the exposure dose of the films was simulated from each position of the powder container, in order to investigate both the contribution from the powder in the same container as the film and the contribution from powder in the other containers (Fig. 5b). The backscattering effect was taken into account by reproducing the lead and copper shielding where the containers were placed during the film exposure.

In order to investigate the difference of the Dr distribution in the samples and the Dr distribution received by the phosphor film, two simulations of a virtual sample made of a K-feldspar half-part irradiating an inert quartz half using the ⁴⁰K beta spectrum were set up: the first with a quartz layer of negligible thickness (1 µm) between two 5mm thick slices of samples (Fig. 5c) in order to determine the natural spreading of Dr in it, the second represents an OSL film protected by an alpha-thick dark low-density polyethylene (PDTE) bag and placed between two 5 mm thick slices of samples (Fig. 5d) in order to observe the Dr spreading resulting from the exposure to beta emissions. The results are compared on Fig. 12.

221 Figure 5

222 3. Results

223 Figure 6

The sensitivity to excitation of the OSL film increases from the 750 nm wavelength, where it is almost negligible, to the 475 nm (Fig. 6). This is in agreement with previous measurements of the Al₂O₃:C excitation spectrum by Chruścińska (2016). Although it seems more efficient to stimulate this phosphor in lower wavelengths around 500 nm, it would be too close to the Al₂O₃:C main emission peaks around 330 nm and 425 nm (Yukihara and McKeever, 2006). This would lead to either significant risk of damaging the photomultiplier or using thick of optical filters reducing the luminescence signal measured.

230 Figure 7

231 The time resolved OSL analysis of the phosphor indicates two slowly decaying components of the 232 luminescence signal, with time constants of 24.0 ± 0.1 ms and 248 ± 13 ms respectively (Fig. 7). These two 233 components where previously measured by Summer (1984) as well as by Markey et al. (1995) to approximatively 234 35 ms, corresponding to the F-center lifetime, and to approximatively 545 ms at 25°C, this second component 235 being temperature dependant according to measurements from room temperature to 100 °C from Markey et al. 236 (1995). Though of the same order of magnitude, the decay constants measured in this study at ambient 237 temperature are significantly shorter than those measured by Markey et al. (1995). The reason for this difference 238 is not clear but will be investigated in further studies.

239 Figure 8

Maps of the luminescence signals from the gamma irradiations (Fig. 8) indicate a homogeneous signal in
 this piece of film, with some statistical variations. A significant background signal can be seen on the blank image;
 this background cannot be bleached either using white light or the laser stimulation.

243 The luminescence signal corresponding to the edge of the film is lower than the signal in the central part, 244 probably resulting from the laser beam stimulating an area overlapping the sample and the support filter For this 245 reason, when integrating the signals from multiple pixels, the outermost 2 pixels (corresponding to an area up to 1 246 mm away from the edge) were not taken into account. The calibration curve resulting from these integrations 247 indicates a linear response of this OSL film to dose (Fig. 9), as was previously observed by Markey et al. (1995). 248 The 2σ uncertainties indicated on the abscise axis results from the quadratic sum of the relative uncertainties on 249 the gamma source calibration and on the exposure time. The uncertainties on the signal counts were calculated 250 as the quadratic sum of the absolute values of the uncertainties on the dark count, on the background counts and 251 on the luminescence counts (whose standard deviation was estimated as the square root of the counts), all 252 integrated over an area of approximatively 35 mm². The final uncertainties remain under 2 % at 2 and therefore 253 cannot be seen on Fig. 9.

254 Figure 9

The dark count integrated over the same area as the OSL signal ranged from 87 to 124 counts per point of measurement (corresponding to a 3 s measurement), with a maximum standard deviation of 18 counts. The average background signal was measured on the blank to 123 counts per point of measurement, with a standard deviation of 10 counts after quadratic subtraction of the dark count standard deviation during this analysis. The limits of detection L_{det} and the limits of quantification L_{qt} are calculated for different surface of integration on Fig. 10. The formula used for calculating these values are:

261
$$L_{det} = 3(\Delta_{DC}^2 + \Delta_{BG}^2)^{0.5} .(N-1)^{-0.5}$$
 (1)

262
$$L_{qt} = 10(\Delta_{DC}^2 + \Delta_{BG}^2)^{0.5} . (N-1)^{-0.5}$$

263 Where Δ_{DC} is the maximum standard deviation of the dark count, Δ_{BG} is the standard deviation of the background 264 measurement, and N is the number of measured points that were integrated. The measurements presented on Fig. 265 9 were integrated over an area of about 560 measurement points, resulting in a L_{det} of 5 µGy and a L_{qt} of 18 µGy.

(2)

- 266 Figure 10
- 267 Table 2

- The simulations calculated a significant attenuation of the beta dose rate, resulting from the shielding by the protective layer and by the substrate of the Al_2O_3 :C as well as from the missing radiation from the volume occupied by the dosimeters and plastic bags (Table 2). This attenuation is different for the different beta spectra. An average value of attenuation factor can be calculated to 0.66 ± 0.01 considering the proportion of radioactive elements in the granulite powder or to 0.65 ± 0.01 considering the proportion of radioactive elements in the basalt powder or in
- a typical sediment (Aitken, 1985). The gamma dose contribution represents 7 % to 8 % of the total exposure dose,
- with 87 % to 58 % of the gamma dose (for the granulite powder and the basalt powder respectively) coming from
- the same container as the film, the rest of the gamma dose contribution coming from the other containers.
- 276 Figure 11

Fig. 11a seems to indicate a linear response to dose of the pieces of film exposed to the powder samples. The lower slope than for the gamma irradiated film results (Fig. 9) may indicates a variability in signal to dose response of the film. The intercept (with a value of 94 ± 31 cps) indicates the environmental dose received by the sample during the time of exposure, corresponding to $304 \pm 99 \,\mu$ Gy, equivalent to a dose rate of $0.23 \pm 0.08 \,\text{mGy.y}^2$ 1. This is compatible with the hard cosmic radiation component at sea level. Fig. 11b shows a good consistency between the calculated exposure doses and the equivalent gamma doses, with a ratio of 1.02 ± 0.07 determined by the slope value.

284 Figure 12

The dose profile obtained from simulation of exposure highlight a difference of spatial distribution between the dose in the sample and the dose received by the phosphor (Fig. 12). This difference is due to the non-negligible thickness of the detector and its cover compared to the average beta range: it represents an inert layer of 272 µm where the beta particles from the sample spread, that will result in an effect comparable to a blurring on the image obtained by laser scan of the dosimeter. Because of this, the beta dose rate image should require a deconvolution or another method in order to take in account the decreasing of apparent variation of the dose rate due to the blurring effect.

292 4. Discussion

This Al₂O₃:C OSL film is sensitive enough to detect sub-mGy doses, with a linear dose response from µGy to mGy levels (Fig. 9 and fig. 11). The significant background signal may limit the accuracy for low dose mapping. Further studies will investigate the possibility of bleaching this background signal using temperature or different stimulation wavelengths. Unfortunately, the polyester nature of the substrate and the binder limit the temperature to the which the film can be exposed.

298 When comparing the OSL signals from the gamma irradiated film (Fig. 9) and the film pieces exposed to 299 the powder samples (Fig. 11a), it appears that the second is about 30% lower for the same dose. Several 300 hypotheses are currently under investigation in order to explain this difference in response. The most likely is that 301 the sample support used for the films exposed to powder was different than the support used for the gamma 302 irradiated piece of film, what put the firsts 3 mm further from the photomultiplier than the second, resulting in a 303 smaller solid angle for the luminescence photon to reach the detector. The comparison between the calculated 304 exposure doses and the equivalent gamma dose shows a good correlation (Fig. 11b), which validates the beta and 305 gamma contributions calculated by simulations (Table 2) and indicates that the sensitivity of the film to gamma 306 exposure is similar to beta exposure.

307 The sub-mGy L_{qt} (422 μ Gy per measurement point) enables the possibility of a pixel-by-pixel calibration 308 of the measurement for long enough exposure time, leading to high resolution mapping of Dr. This L_{qt} can be 309 brought under 100 mGy by integrating areas of about 20 pixels, in order to limit the time of exposure to sample to 310 a few weeks. This corresponds to areas of 5 mm² for 500 μ m pixels (equivalent to a resolution of 2.24 mm) or 0.45 311 mm² for 150 μ m pixels (equivalent to a resolution of 0.67 mm). A strategy to benefit from this would be to identify 312 the homogeneous areas and to integrate the signal over these, in order to lower the L_{qt} and to increase the accuracy of the Dr measurement for these areas. However this may not be always possible in the case of heterogeneous sample exposure. It is always possible to obtain higher resolutions and accuracy by longer exposure time, or with sample with a higher radioactivity such as granite and granulite.

316 The environmental background Dr during exposure is another parameter that can limit the accuracy of the 317 measurement. Fig. 11 shows that it is necessary to set up a blank in order to measure this environmental Dr 318 contribution, but it is better to shield against environmental radiation as much as possible to preserve the accuracy 319 of the measurement. Samples under exposure can be placed in containers thick enough to shield them from beta 320 radiation from other samples. The use of a lead shield can efficiently cut the gamma radiation and the soft 321 component of cosmic radiation, while X-rays from atomic deexcitation and from Bremsstrahlung radiation can be 322 efficiently shielded using inert copper. Using such shielding, we can see on fig. 11 that the environmental 323 background can be reduced to about 0.23 ± 0.08 mGy.y⁻¹, which is the order of magnitude of the hard component 324 of cosmic radiations at sea level. Unfortunately, this is still enough to produce OSL signal of the same order of 325 magnitude as the dark count of the photomultiplier or as the observed background signal of the Al₂O₃:C film. This 326 would lead to higher limit of detection and quantification, significantly reducing the accuracy of sub-mGy level 327 measurements.

328 The reduction of the highly penetrating cosmic radiation component is more problematic as it needs 329 several meters of rock to be significantly attenuated. In order to benefit from an environment extremely clean from 330 cosmic radiation, OSL film exposures to granulite slices are currently underway in the STFC Boulby Underground 331 Laboratory (Saltburn-by-the-Sea, UK). This laboratory is built 1.1 km underground, efficiently reducing the cosmic 332 radiation Dr to a negligible level with a muon reduction factor of 10⁶ (Murphy and Paling, 2012). Each sample and 333 film were placed in pure quartz containers of 1 mm thickness, so each is separated from surrounding samples by 334 2 mm of guartz which is enough to absorb more than 99% of the natural beta radiation. The samples are shielded 335 from X-rays and gamma radiation by pure copper bricks of 5 cm to 10 cm thickness (Fig. 13a) and by a 20cm thick 336 Zeplin lead shield (Fig. 13b).

337 Figure 13

338 The simulation results from Fig. 12 point out a major issue of the beta dose rate imaging: the dose 339 distribution on the image can be different from the dose distribution in the sample, depending on the detector 340 characteristics and geometry. This may indicate that the quantification of beta dose rate distribution from previous 341 studies that did not consider this effect may be biased (Romanyukha et al. 2017; Smedley et al., 2020); in particular 342 the beta dose rate dispersion could be underestimated. It is noticeable that even if the distribution of the dose 343 received in the phosphor is different than in the sample, the calibrated dose value resulting from the integration 344 over the whole sensitive area (with the exclusion of the edge potentially affected by edge effect) should be the 345 same (equal to half of the infinite matrix dose of the radioactive part in the case of this modelling). The only 346 difference is the higher spreading of the beta in the detector, resulting in what could be described as a "blurring 347 effect" in the imaging of the dose distribution. Simulations adapted to the geometry of sample exposure could be 348 used to calculate deconvolution parameters, such as point spread functions, in order to deconvolve the dose image 349 for reconstructing the dose distribution in the sample.

350 5. Conclusion

This study demonstrates the high potential of Landauer's Al_2O_3 :C OSL dosimeter films for imaging the beta dose rate, in combination with the developed protocol of laser scanning pulsed OSL and with Monte Carlo simulation for calculating attenuation factors and eventual deconvolution parameters. It presents a linear dose response from µGy to mGy level, and a limit of quantification per point in the sub-mGy level. Quantification below 100 µGy can be achieved by integrating over a few pixels. This is enough to obtain an accurate Dr image of natural samples over a few weeks to a few months of exposure time, especially if benefiting from a very low environmental background such as is reachable in underground laboratories. A high resolution of 150 µm can be achieved using

- 358 the described laser scanning OSL reader, but the necessity to integrate the signal over several pixels in order to 359 reach an acceptable accuracy may reduce this resolution for low dose exposure.
- Experiments are currently under way in order to test the imaging of beta dose rate of heterogeneous samples. It will benefit from the ultra-low environmental background reachable at the STFC Boulby Underground Laboratory, and of image deconvolution processing with parameters obtained from the beta simulation results. Future work will also apply the techniques described here to rock samples.
- 364

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Figure 1 (1.5 column): Geometry and composition of the Landauer Al₂O₃:C OSL film

Figure 2 (single column): excitation spectrometer schematic



Figure 3 (single column): Time resolved OSL reader schematic



Figure 4 (single column): Laser scanning imaging OSL reader schematic



Figure 5 (single column): Geometries of the Geant4 simulations

a - Dosimeter exposure to powdered sample



b - Sample containers in the environmental radiation shield



c -Dose rate distribution in a K-feldspar-Quartz sample



d - Dosimeter exposure to a K-feldspar-Quartz sample



Figure 6 (single column): Excitation spectrum of the Al₂O₃:C film



Figure 7 (single column): Pulse stimulated OSL of the Al_2O_3 :C film. The pulse duration is 130ms and the delay between pulses is 1500ms. The signal decay after the pulse is best fitted by a double exponential decay with half-time constants of 24.0 \pm 0.1 ms and 248 \pm 13 ms



Figure 8 (2 columns): OSL imaging of a piece of Al_2O_3 :C film. The dark counts were not subtracted. The background from the sample support can be observed around the piece of film and is not significantly higher than the dark counts value, indicating that there is no significant scattering of the laser beam nor luminescence from the support. A high-count pixel can be seen out of the film area, near the top right corner of the 295 μ Gy image. Its origin is under investigation and they are removed from analysis when occurring in the film area. It can be seen that the piece of film lightly shifted between scanning, due to the support that have been improved since.



Figure 9 (1.5 column): OSL signal of piece of Al₂O₃:C film irradiated by a ⁶⁰Co gamma source. *The uncertainties on the gamma dose are provided at the 95% confidence level. The uncertainties on the average counts per pixel are negligible.*





Figure 10 (single column): Detection and quantification limits for a piece of Al₂O₃:C film

Figure 11 (1.5 column): Calibration curve and comparison of calculated dose with equivalent gamma dose. The counts were averaged over the whole surface of the dose image recorded by the dosimeter except the edges, for a total of about 5500 pixels of 250 μ m per image. The dark count and the phosphor background signal were subtracted from the results of graph a, so the remaining offset of 94 ± 31 cps corresponds to the environmental background dose. This environmental background was additionally subtracted for graph b in order to highlight only the relation between calculated doses and equivalent gamma doses. The uncertainties on the calculated dose are provided at the 95% confidence level.



a - OSL signal from exposure of dosimeter film pieces to powder samples. The uncertainties on the average counts per pixel is inferior to 1%.

b – Comparison of the calculated dose for each sample exposure with the equivalent gamma dose. The additional uncertainty on the normalized dose is due to the uncertainty on the gamma source dose rate (145 ± 7 μ Gy.h⁻¹)





Figure 12 (1.5 column): beta dose profiles from Geant4 simulations

Figure 13 (single column): Environmental radiation shielding at the STFC Boulby Underground Laboratory

a-5 cm thick copper brick shielding



b - Zeplin lead shield



 Table 1 (single column): Radioactive element contents in the powder samples. The uncertainties are provided at the 95% confidence level.

Powder composition	K content	U content	Th content	
	(wt.%)	(ppm /	(ppm /	
		mg.kg ⁻¹)	mg.kg ⁻¹)	
Granulite 100%	3.46 ± 0.06	6.90 ± 0.12	16.9 ± 0.3	
Granulite 75% - Basalt 25%	2.71 ± 0.05	5.50 ± 0.11	13.7 ± 0.2	
Granulite 50% - Basalt 50%	1.96 ± 0.04	4.09 ± 0.10	10.5 ± 0.2	
Granulite 25% - Basalt 75%	1.21 ± 0.03	2.69 ± 0.09	7.35 ± 0.2	
Basalt 100%	0.46 ± 0.02	1.28 ±0.08	4.2 ± 0.1	

 Table 2 (single column): beta dose rate attenuation during dosimeter film exposure to powder samples. These

 values were calculated by simulation. The uncertainties are provided at the 95% confidence level.

spectra	Beta attenuation factor*	Gamma dose rate
		contribution*
⁴⁰ K	0.680 ± 0.002	0.0402 ± 0.0006
U-series	0.638 ± 0.001	0.1447 ± 0.0004
Th-series	0.581 ± 0.001	0.1169 ± 0.0004
Granulite **	0.66 ± 0.01	0.101 ± 0.001
Basalt **	0.65 ± 0.01	0.169 ± 0.002
Typical sediment ***	0.65 ± 0.01	0.128 ± 0.001

* Given as ratio of the corresponding infinite matrix dose rate of the sample

** See table 1 for radioactive element contents

*** ⁴⁰K 1 %, U 3 ppm, Th 10 ppm (Aitken, 1985)