

McGinn, B.J., and Morrison, J.D. (2016) Investigations into the absorption of insulin and insulin derivatives from the small intestine of the anaesthetised rat. *Journal of Controlled Release*, 232, pp. 120-130. (doi:<u>10.1016/j.jconrel.2016.04.002</u>)

This is the author's final accepted version.

There may be differences between this version and the published version. You are advised to consult the publisher's version if you wish to cite from it.

http://eprints.gla.ac.uk/120651/

Deposited on: 6 July 2016

Enlighten – Research publications by members of the University of Glasgow http://eprints.gla.ac.uk

Investigations into the absorption of insulin and insulin derivatives from the small intestine of the anaesthetised rat

B.J. $McGinn^1$ & J. D. $Morrison^2$

¹ Thistle Research, Westbourne Crescent, Glasgow G61 4HB, Scotland

 2 School of Life Sciences, West Medical Building, University of Glasgow, Glasgow G12 8QQ, Scotland

Short title Absorption of cholyl-insulin

 $Key\ words:$ Insulin, insulin decapeptide, cholyl-insulin, cholic acid, ileum, jejunum, absorption

Chemical compounds studied in this article:

Human recombinant insulin (PubChem CID: 90488846); Bovine insulin (PubChem CID: 16131099); Cholic acid (PubChem CID: 221493); Sodium taurocholate (PubChem CID: CID: 23666345); A21,20-S-S-B19-26 insulin decapeptide; B¹⁹-Cys-cholyl-insulin decapeptide; B²⁹-Lys-cholyl-insulin; B¹-Phe-cholyl-insulin

Corresponding author

J.D. Morrison, West Medical Building, University of Glasgow, Glasgow G12 8QQ, Scotland.

Telephone: 0141 330 4073 email: James.Morrison@gla.ac.uk

ABSTRACT

Experiments have been undertaken to determine the extent to which cholic acid conjugates of insulin were absorbed from the small intestine of anaesthetised rats by means of the bile salt transporters of the ileum. The measure used to assess the absorption of the cholyl-insulins was the amount of hypoglycaemia following infusion into the small intestine. Control experiments involving infusion of natural insulin into the ileum showed either nil absorption or absorption of a small amount of insulin as indicated by transient dip in the blood glucose concentration. However, when insulin was co-infused with the bile salt taurocholate, this was followed by a marked hypoglycaemic response which was specific to the ileum and did not occur on infusion into the jejunum. When the two cholyl conjugates of insulin were tested viz. B^{29} -Lys-cholyl-insulin and B^{1} -Phe-cholyl-insulin, both were biologically active as indicated by hypoglycaemic responses on systemic injection, though their potency was about 40% of that of natural insulin. While there was no evidence for the absorption of B²⁹-Lys-cholyl-insulin when infused into the ileum, B¹-Phe-cholyl-insulin did cause a long lasting hypoglycaemic response, indicating that absorption had occurred. Since the hypoglycaemic response was blocked on co-infusion with taurocholate and was absent for infusion of the conjugate into the jejunum, these results were taken as evidence that B¹-Phe-cholyl-insulin had been taken up by the ileal bile salt transporters. This would indicate that B¹-Phe-cholyl-insulin is worthy of further investigation for use in an oral insulin formulation.

1. Introduction

Since its discovery in 1922, the hormone insulin has been administered by sub-cutaneous injection for the treatment of diabetes mellitus (Type 1) which arises from the loss of the β -cells of the Islets of Langerhans of the pancreas and the subsequent loss of insulin production [1]. The diabetic patient suffers not only from uncontrolled blood glucose levels but also, in the longer term, from vascular disease due to glycosylation of haemoglobin. To this end, more intensive therapy involving at least 3 injections of insulin each day has been shown to be beneficial in reducing the incidence of retinopathy and nephropathy [2]. Compliance can, however, be compromised by an aversion to self-injection due to discomfort, abscess formation, scarring and lipohypertrophy at the site of injection [3]. Hence, alternative methods of treatment in the form of power injection of insulin into the skin with pressurised helium gas [4], through inhalation of fine particles of insulin for absorption from the alveoli [5] and through pancreatic islet cell transplantation [6] have been developed, though none of these has proved to be a successful replacement for insulin injections. The most desirable method of delivery would be an oral formulation taken at meal-time, though this is fraught with several major considerations. First, there is the need for protection of the orally-ingested insulin against digestion by gastro-intestinal proteases [7, 8, 9, 10]. Then, once delivered into the small intestine, there then arises the not inconsiderable problem of promoting the absorption of such a large charged molecule which consists of an A chain of 21 amino acids joined by 2 disulphide bridges to a B chain of 30 amino acids, across the intestinal mucosa into the mucosal circulation. This would have to occur repeatedly for several applications of the formulation per day, extending over the individual's life time, without the risk of cumulative damage to the intestinal mucosa. Of critical importance would be the quantity and the timing of ingestion of the formulation relative to the meal to be consumed. Long term safety in terms of the toxicology of the insulin delivery system and the innocuousness of non-absorbed insulin in the colon would also need to be assured [11]. While an oral insulin formulation is beset with many difficulties, there have nevertheless been numerous efforts over the past decades towards reaching this goal. The consensus is that absorption of insulin from the small intestine, when infused in a moderate dose in a saline vehicle, does not occur to any significant extent in animal models [12, 13, 14, 15, 16, 17, 18 19, 20, 21, 22, 23, 24, 25, 26, 27, 28, 29, 30, 31, 32, 33, 34], though some uptake has been reported for jejunal and ileal infusions in conscious rabbits [35] and with high luminal doses in rabbit [30] and in rat [26, 36]. In the promotion of insulin uptake, the approaches can be divided broadly into the promotion of delivery of natural insulin to maximise its concentration at the small intestinal mucosa and through the uptake of covalently-bonded insulin.

1.1. Promotion of absorption of natural insulin

There have been numerous investigations involving different insulin formulations with the purpose of promoting the absorption of natural insulin from the small intestine, as shown in the summary presented in Table 1. In addition, there are also published results of clinical trials which do not impart specific details of the formulation adopted *e.g.* ORMD-0801 [37] and there is some limited information available from the web sites and press releases of pharmaceutical companies [38]. In general, the published results for the different insulin carrier systems, with one exception in which insulin uptake was reported only from the colon [33], have indicated considerable success. This is exemplified by the outcome of the 36 studies involving animal models in which infusion of the insulin formulation into the small intestine *in vivo* led to a reduction in the blood glucose concentration by 49 ± 3 % with a duration of action of 3.4 ± 0.4 h (mean \pm S.E.M.).

The routes by which insulin is absorbed across the small intestinal mucosa may be transcellular or paracellular. The small intestinal epithelium consists of about 90% enterocytes and 10% goblet cells which secret mucus. These are joined at their luminal border by tight junctions which consist of interleaving loops of the protein occludin which can be regulated to increase the pore diameter of the junctions [39]. In the ileum, there are also M cells (membranous epithelial cells) which overlie the Peyer's patches and which are known to be able to take up macromolecules from the lumen [40]. Immunocytochemical studies suggest that the major route for absorption of free insulin is by the transcellular route through the enterocytes [41] in which macromolecules are taken up at the luminal membrane by phagocytosis or pinocytosis followed by exocytosis at the basolateral membrane and absorption into the mesenteric circulation [42]. This route of absorption is facilitated by co-infusion of insulin with cell-penetrating peptides [23, 43, 44] and bile salt liposomes [45]. In addition, there may be uptake through pores in the mucosa which form transiently as a consequence of the shedding of the enterocytes at the tips of the villi [46]. By contrast, insulin nanoparticle absorption has been described as occurring by the paracellular route through the tight junctions and intercellular clefts [47, 48, 49] and this process is enhanced by permeant inhibitors of phosphatase [31]. However, it has been claimed that, while nanoparticles do provide protection against the action of intestinal proteases, there was no resulting enhancement of absorption [50]. Also, the paracellular route is not the only means of absorption since lauryl succinyl chitosan also passes

transcellularly [25], while poly(- ϵ -caprolactone) is absorbed specifically by the Peyer's patches [51] and, in the case of vitamin B₁₂-linked nanoparticles, absorption would be by the vitamin B₁₂ transporters which are located in the ileum [52].

Table 1

Summary of strategies to promote absorption of natural insulin

	Vehicle	Constituent	References
(i)	Saline vehicle	apoprotinin ¹	[20, 33, 34, 53]
		bile salts	[20, 33, 34, 53, 54]
		bile salts and apoprotinin	[34, 41, 53, 55]
		bile salts and bicarbonate	[54]
		bile salts and fatty acid mixed micelles	[29, 56]
		bile salts, palmitic acid, tocopherol	[19]
		caproic acid	[20]
		cetomacrogol or 5-methoxysalicylate ²	[27, 32]
		hyaluronic acid	[57, 58]
		$hyaluronidase^3$	[21]
		oligo-arginine, penetratin ⁴	[23, 43, 44]
		permeant inhibitor of phosphatase	[31]
		phenylalanine derivatives	[12]
		zonulin occludin toxin ⁵	[18]
(ii)	Enteric-coated	calcium phosphate	[59]
		cellulose acetate phthalate	[60, 61, 62]
		gelatin	[63]
(iii)	Liposomes	glycocholate	[24]
		red cell ghosts or liposomes	[11, 36]
(iv)	Water/oil/water	micro-emulsions	[9, 46]
	emulsions	saturated or unsaturated fatty acids	[17, 30, 64]
		4CNAB^6	[38, 65]
(\mathbf{v})	Nano/micro	chitosan	[66]
	particles	chitosan/poly(γ -glutamic acid)	[48, 63]
		cyclodextrin polymethacrylic acid hydrogel	[28]
		hyaluron-coated fibrillar insulin	[16]
		isobutyl-2-cyanoacrylate	[67, 68]
		lauryl succinyl chitosan	[25]
		phosphatidylcholine	[69]
		poly(lactic acid)-pluronic acid	[70]
		polymethacrylic acid polyethylene glycol	[22]
		$poly(-\epsilon$ -caprolactone)	[51]
		polymerised fumaric acid and sebacic acid	[71]
		trimethyl chitosan	[49]
		vitamin B_{12} -linked dextran-epichlorohydrin	[15]
		vitamin B_{12} -linked polyallylamine	[72]

 1 protease inhibitor, 2 surfactants, 3 pretreatment to degrade glycocalyx overlying mucosal epithelial cells, 4 cell-penetrating peptides, 5 to open tight junctions, 6 monosodium N-(4-chlorosalicyloyl)-4-aminobutyrate

1.2. Absorption of covalently-bonded insulin

Investigations involving the absorption of covalently-bonded molecules have consisted of the following.

(i) Insulin has been conjugated at its B^1 -NH₂ group or at both the B^1 and B^{29} NH₂ groups with palmitic acid [73], caproic acid [13] and methoxy-polyethylene glycol (PEG) [14] in order to increase lipid solubility in the enterocyte luminal membrane.

(ii) Conjugation of customised peptides at the C³ hydroxyl group of cholic acid has been made with the purpose of promoting uptake by the bile salt transporters which are located in the ileum [74]. This, however, was successful only for peptides of up to ten amino acids [75]. Conjugation has also been undertaken at the C²⁴ carboxyl group *via* a γ glutamyl link, though uptake was limited to tetrapeptides and hexapeptides [76].

(iii) Direct conjugation to the C^{24} carboxyl group of cholic acid has been undertaken with triiodothyronine, though the purpose in this case was to reduce the uptake by the heart since triiodothyronine is already absorbable from the small intestine [77]. Successful absorption of a carbohydrate molecule in the form of heparin which was conjugated at an amine group to the C^{24} carboxyl group of deoxycholic acid has also been reported [78].

In our experiments into the absorption of gastro-intestinal hormones from the small intestine of anaesthetised rats, we conjugated the hormone directly to the C^{24} carboxyl group of cholic acid. Conjugation was made directly to the N terminus of the 34 amino acid hormone gastrin which stimulates gastric HCl secretion [79] and the 27 amino acid hormone secret in which stimulates pancreatic HCO_3^- secretion [80]. Conjugation had the effect of increasing the biological activity of gastrin while that of secretin was reduced. However, in both cases, appreciable absorption of the cholyl-gastrin and cholyl-secretin was recorded with the latter achieving a bio-availability of 20-37% [80]. Since the uptake was specific to the ileum and did not occur from the jejunum and since it was blocked by co-infusion with taurocholate which was used as a competitive inhibitor, we concluded that the cholyl hormone derivatives had been absorbed by the bile salt transporters. It is this approach which we now extend to the absorption of cholyl-insulin. In the initial experiments, we investigated the A21,20-S-S-B19-26 decapeptide of insulin and its B¹⁹-Cys-cholyl-derivative since these were amenable to chemical synthesis and the insulin decapeptide has been reported to possess 77% insulin activity [81]. However, the decapeptides proved to be devoid of biological activity and, so, we then tested the extent to which there was absorption of the cholyl derivatives of the full insulin molecule which possesses three free $-NH_2$ groups. Since the A¹-Glycine residue is required for hormone activity [82], we tested the absorption of, first, B²⁹-Lys-cholyl-insulin and, second, B¹-Phe-cholyl-insulin. Experiments were also undertaken to assess the absorption of natural insulin in order to provide a reference for the cholyl-insulin experiments.

2. Materials and methods

2.1. Surgical procedures

Experiments were carried out on male Wistar rats, weight 240-360 g in accordance with the Animals (Scientific Procedures) Act 1986. The animals were fasted overnight but were allowed a 5% sucrose drink in addition to water. They were anaesthetised with an intra-peritoneal (I.P.) injection of pentobarbitone sodium (Rhône Mérieux, Harlow, UK) at a dose of 80 mg kg⁻¹. The criterion for anaesthesia was abolition of the hind limb flexor withdrawal reflex. In order to maintain the level of anaesthesia, supplementary I.P. injections (24 mg kg⁻¹) were given as required. At the end of the experiments, the animals were killed with an intra-venous (I.V.) or intra-arterial (I.A.) injection of 100 mg Euthatal (Merial Animal Health, Harlow, UK).

The initial surgical procedures consisted of tracheostomy to allow tracheal aspiration and artificial ventilation, if necessary, and cannulation of the carotid artery with a Portex cannula of outer diameter 1.0 mm to monitor the arterial blood pressure. This was followed by cannulation of the external iliac vein with a cannula of outer diameter 1.0 mm or of the external iliac artery with a cannula of outer diameter 0.75 mm in order to allow blood sampling or injection of hormones. The cannulae contained heparinised saline at 100 I.U. heparin ml^{-1} (Leo Laboratories Ltd., Princes Risborough, UK). After a midline laparotomy, the pyloro-duodenal junction was ligated to prevent entry of gastric contents into the duodenum and hence the possible release of duodenal hormones. The terminal ileum was cannulated with a perforated Portex cannula of 2.0 mm outer diameter which extended from a point of entry in the wall of the proximal colon through the ileo-colic junction into the ileum. The ileum was then gently infused under visual observation with 0.5 mL saline solution at 37°C, which was followed by slow withdrawal to remove any bile and residual digestive matter. This process was repeated until the effluent was clear. In some cases, an outlet cannula of 4 mm outer diameter was inserted 15 cm from the inlet cannula to facilitate flushing. When jejunal cannulation was required, this was undertaken with a perforated Portex cannula of 2.0 mm outer diameter with a point of entry just distal to the ligament of Treitz. In these cases, the small intestine was also ligated *ca.* 30cm from the ileo-colic junction to prevent entry of the jejunal infusate into the ileum. The jejunum was also flushed with warm saline solution to remove the luminal contents. Some animals had both ileal and jejunal loops. Finally, bilateral cervical vagotomy was undertaken to remove vago-vagal reflexes. The animal's temperature was maintained as near as possible to 37°C and, at the end of the experiment, samples of the ileal/jejunal loops were taken for histology.

2.2. Blood samples

Blood glucose measurements were made in duplicate, with further samples taken if the duplicates differed appreciably, using the Accu-Chek glucose meter (Roche Diagnostics, Burgess Hill, UK) which was calibrated with the manufacturer's calibration solutions. Blood samples were obtained initially from the external iliac artery or vein and then by incision of the tail artery. In the former, 2 small samples of 0.2 mL blood were withdrawn

and the second sample was assayed: unused blood was then returned followed by a small saline flush. In the latter, the first drop of blood was removed and the second drop assayed. The incision was then sealed with surgical tape. In 4 experiments, sufficient blood was withdrawn systemically to allow a parallel photometric assay using glucose oxidase and dianisidine (Sigma GAGO-20,; Sigma, Poole, UK). For 40 samples with a range of glucose concentrations of 0.5 to 9 mM, there was strong correlation between the two assays (r = 0.96, P < 0.001), which confirmed the suitability of the Accu-Chek glucose meter. In 7 experiments, one of which is shown in Fig. 1, comparisons were made between parallel Accu-Chek glucose readings covering a range of 2 to 9 mM taken from 21 pairs of deep arterial and tail artery samples. These also showed a highly significant correlation (r = 0.99, P < 0.001) and confirmed the suitabily of tail artery sampling which had the advantage of causing less disturbance to the arterial blood pressure.

2.3. Injections and infusions

I.A. or I.V. injections of hormones were made with the hormone dissolved in 0.1 mL saline and were followed by 0.2 mL saline to flush through the cannula. For intra-ileal or intra-jejunal infusions, the appropriate weight of hormone was dissolved in 1.0 ml saline which was either phosphate buffered saline (147 mM NaCl, 3.0 mM Na₂HPO₄) or citrate-phosphate saline (144 mM NaCl, 3.0 mM Na₂HPO₄, 1.0 mM citric acid) with the purpose of chelating any zinc ions to preclude the possibility of hexamer formation [83]. The pH of the saline was set to 8.2 at a temperature of 37°C and was infused slowly over a period of 3 min when it was followed by a wash-in infusion of 0.2 ml saline. In control experiments, slow infusions of 1.0 mL saline at pH 8.2 were also made. The rate of absorption of fluid from the intestinal loop was also monitored by visual inspection at 30 min intervals. In some experiments, co-infusions were made with 20 mM sodium taurocholate (Sigma T-4009) which is the main bile salt in the rat [84], with the dose of 20 mM being at the lower end of the normal range in natural bile [85]. Protease inhibitors were not used in the experiments.

2.4. Insulin conjugates

Since insulin is a highly conserved hormone with only small differences between species [86], we were not constrained by the source of the insulin and control experiments were made with human recombinant insulin, molecular weight (MW) 5808 (Sigma I-9278). Cholyl-insulin, MW 6124, was manufactured by the conjugation of bovine insulin (Sigma I-5500) to cholic acid N-hydroxysuccinimide ester. Dimer and hexamer insulin self-association was prevented by use of a citrate buffer. Conjugation with the C^{24} carboxyl group of cholic acid was achieved at the B^1 -Phe NH₂ residue by setting the insulin buffer solution at pH 8.5 and at the B^{29} -Lys NH₂ residue with pH 10. Addition of small aliquots of cholic acid-N-hydroxysuccinimide ester to the bovine insulin was followed by the appropriate aliquots of NaOH solution which was used to maintain the pH throughout the conjugation reaction. When an analytical hplc indicated the optimum reaction yield of mono-conjugated insulin, the reaction was stopped and the cholyl-insulin precipitated by acidification with HCl to pH 2-3. Preparative reversed-phase hplc was employed to recover pure mono-conjugate and remove unconjugated and multiple conjugated insulin. The purified material was freeze-dried and stored at -20°C. Insulin decapeptide (I10)

(A21,20-S-S-B19-26, MW 1210)) and cholyl-insulin decapeptide (B¹⁹-Cys-cholyl-I10, MW 1600) were synthesised *de novo* by polymer-supported peptide synthesis techniques [79]. The MW of I10 and the cholyl-insulins was confirmed by mass spectrometry (MS) and identification of the cholate binding site was undertaken by MS analysis of the products of trypsin digest of the cholyl-insulin molecules.

2.5. Histology

As a standard procedure in the intestinal infusion experiments, a 5 cm length of small intestine was resected immediately after termination of the experiment, infused with 10% formal saline and immersed in 10% formal saline overnight. The tissue was then processed for paraffin embedding and transverse sections were made at several locations in each segment of gut. These were stained with haematoxylin/eosin and alcian blue for light microscopy.

2.6. Data analysis

In addition to representative experiments from single animals, group results are presented for the intestinal infusion experiments in the form of the mean \pm S.E.M. normalised to a control blood glucose concentration of 5.0 mM. Following an experimental procedure, the hypoglycaemic response was measured as the decrement in the blood glucose concentration from the preceding baseline for each 15 min test period over the duration of the response. If, instead of a level baseline, there was progressive hyperglycaemia, *e.g.* Fig. 1, the response was obtained as the decrement from the best fitting regression line derived from data values which occurred prior and subsequent to the response. An overall response- the cumulative response- was then calculated as the summation of the decrements at each 15 min test period. Tests against zero were made with the *t*-test while comparisons of results between cohorts of animals were made with the two sample *t*-test and within cohorts of animals with the paired *t*-test. Linear regression analysis was undertaken to compare two sets of variables. The analyses were undertaken with Minitab 15 (Minitab UK, Coventry, UK) and statistical significance was taken as P < 0.05.

3. Results

The present results were obtained from experiments of duration 6-8 h from a total of 114 rats in which the mean blood glucose concentration at the commencement of the experiments was 5.1 ± 0.10 mM (mean \pm S.E.M.). The abbreviations which have been employed are: I.A. intra-arterial, I.V. intra-venous, I10 insulin decapeptide, I51 natural insulin. The doses for systemic injections are given as nmol kg⁻¹ while, in the specific experiments illustrated in the Figures, the dose is that which was actually injected into the animal in μ g. The results are expressed throughout as the mean \pm S.E.M.

The arterial blood pressure at the commencement of the experiments had mean systolic/diastolic values of 130/98 mmHg. The mean arterial blood pressure showed a modest but significant reduction from 109 ± 1.36 mmHg at the commencement to 92 ± 1.67 mmHg at 5-8 h later (P < 0.001), while the corresponding values for the pulse pressure of 32 ± 0.9 mmHg and 33 ± 1.3 mmHg were not significantly different (P = 0.45). There was no discernible vascular action of insulin or cholyl-insulin when injected I.A. or I.V. since the arterial blood pressure remained unaffected.

3.1. Control experiments



Fig. 1. Representative control experiment from a single animal showing the blood glucose levels (mM) while 3 intra-ileal infusions of 1.0 mL saline were given at 2 h intervals (S and vertical dashed lines). Blood glucose values were obtained from both the tail artery (solid circles) and the external iliac artery (inverted open triangles). The hyperglycaemic increase between 240 and 360 min has superimposed upon it the line of best fit which was highly significant ($R^2 = 99.4\%$, $P_{slope} < 0.001$).

Control experiments were undertaken in which the blood glucose concentration was followed in the absence of experimental intervention in 5 animals and when intra-ileal infusions of 1.0 mL saline were made during the course of the experiment in a further 2 animals (Fig. 1). The results were very similar in the 7 animals in that, after an initial decline to a steady level, the blood glucose concentration remained reasonably constant over the subsequent 2-3 h, after which it showed a slow progressive linear increase resulting in an elevation of the blood glucose concentration by 1-3 mM after a further 3-4 h. Fig. 1 also shows the close agreement between blood glucose concentrations obtained from sampling from the tail artery and the external iliac artery.

3.2. Systemic injections

From preliminary dose-response experiments with systemic injections of the cholyl-insulins I.A. or I.V., the minimum dose which evoked a discernible response was determined to be 1 nmol kg⁻¹. From this we set our two standard doses at 2 nmol (0.33 I.U.) kg⁻¹ and 20 nmol (3.3 I.U.) kg⁻¹ so as to allow the hypoglycaemic activity of the cholyl-insulins to be compared with that of natural insulin: the results are summarised in Table 2. As to be expected, systemic injection of 2 nmol kg⁻¹ natural insulin, which in this case was human recombinant insulin, caused a marked hypoglycaemic response which, for 8 animals, had a mean maximum reduction of -2.9 \pm 0.20 mM and a duration of $1\frac{1}{2}$ h. At the 20 nmol kg⁻¹ dose, the hypoglycaemic response increased to -4.1 \pm 0.31 mM with a prolonged duration which was in excess of 3 h (Fig. 2a).



Fig. 2. Representative experiments from 4 different animals showing the effects on the blood glucose concentration (mM) of I.A. injections of (a) insulin (I51), (b) insulin decapeptide (I10), (c) B²⁹-Lys-cholyl-I51 (B²⁹CI) and (d) B¹-Phe-cholyl-I51 (B¹CI). The I.A. injections were at doses of 2.0 nmol kg⁻¹ and 20 nmol kg⁻¹ with the exception of I10 (b) when the dose was 1.0 μ mol kg⁻¹. In (b), the responsiveness of the preparation was confirmed with an I.A. injection of 3.5 μ g I51.

By contrast, neither insulin decapeptide (I10) nor cholyl-I10 showed any response to the two standard doses. Even when the dose was increased to 1.0 μ mol kg⁻¹ in 6 animals, there was an absence of response to both I10 and cholyl-I10. Fig. 2b shows an example

of an experiment with I.A. injection of I10 and is equally representative of the outcome of the cholyl-I10 experiments. In all experiments, the responsiveness of the preparation was confirmed from the response to 2 nmol kg⁻¹ insulin I.A.

Table 2

Maximum and cumulative reductions in blood glucose concentration in response to standard doses of insulin and cholyl-insulin I.A.

		2 nmol kg^{-1}	2 nmol kg^{-1}		20 nmol kg^{-1}
	n	$Maximum \ mM$	Cumulative mM	n	Maximum mM
I51	8	$-2.9\pm0.20~\mathrm{mM}$	$-11.4 \pm 1.3 \text{ mM}$	8	$-4.1\pm0.31~\mathrm{mM}$
B ²⁹ -Lys-cholyl-I51	6	$-1.4 \pm 0.22 \text{ mM}^{**}$	$-4.9 \pm 0.6 \text{ mM}^{**}$	6	$-5.0 \pm 0.74 \text{ mM}^+$
B ¹ -Phe-cholyl-I51	6	$-1.5 \pm 0.22 \text{ mM}^{**}$	$-4.0 \pm 1.0 \text{ mM}^{**}$	6	$-4.2 \pm 0.27 \text{ mM}^+$

Reductions in blood glucose concentration indicated by negative values of the mean \pm S.E.M. Results are presented in terms of the maximum depression to each of the two doses and as the cumulative response to the lower dose. The results for each conjugate were compared to the insulin response with the two sample *t*-test: $^+P > 0.30$, $^{**}P < 0.01$.

Both the two choic acid conjugates of the full insulin molecule, viz. B²⁹-Lys-cholyl-I51 and B¹-Phe-cholyl-I51, were biologically active, though with reduced efficacy compared to that of natural insulin (Figures 2c & d, Table 2). In the 6 experiments in which the 2 nmol kg⁻¹ dose was tested, the magnitude of the hypoglycaemic response in terms of the cumulative depression of blood glucose was some 40% of that of natural insulin (P < 0.01). By contrast, when the dose was increased to 20 nmol kg⁻¹ (6 experiments), the magnitude of the hypoglycaemic response to both conjugates increased markedly so that it became indistinguishable from that caused by natural insulin (P > 0.30). The response durations for both conjugates were also prolonged at this dose and were comparable to the durations for natural insulin (Fig. 2).

3.3. Intestinal infusions of insulin

Natural insulin at a dose of 0.7 mg (0.12 μ mol) dissolved in 1.0 mL of phosphate buffered saline at pH 8.2 was infused into the terminal ileum of 11 animals and the effects on the blood glucose concentration was followed over several hours. These experiments were undertaken after lavage of the ileum to remove any residual bile and, in some experiments, the infusate also contained 1.0 mM citric acid to act as a Zn²⁺ chelating agent. The normalised mean data showed a transient reduction in blood glucose concentration over the period 30-75 min after infusion (Fig. 3) which was reflected in a small but significant reduction in the cumulative blood glucose concentration of -2.2 ± 0.9 mM (P = 0.034, Table 3). Further analysis, however, revealed 2 groups of results. In 6 animals, there was an absence of a response (Fig. 4a) as confirmed by the non-significant cumulative response of -0.3 ± 0.2 mM (P = 0.13) while in 5 animals, there was a significant cumulative response of -4.4 ± 1.42 mM (P = 0.036) which extended over 60-90 min (Fig. 4b). There was, however, no ostensible reason for this dichotomy in that both groups showed an intact mucosa under light microscopy, the time course of fluid absorption was normal with a flaccid state being reached after 2 h, and there was no difference as to whether phosphate buffered saline or citrate/phosphate buffered saline was employed. In a further 7 experiments, the intra-ileal dose of insulin was increased to 2.7 mg (0.50 μ mol) with the outcome that 6 animals showed zero response while one animal showed a small hypoglycaemic dip of -1.2 mM over 30 min. Hence, overall, the outcome from these experiments is that natural insulin is not generally absorbed from the ileum though, occasionally, a small quantity may enter the systemic circulation.



Fig. 3. Mean \pm S.E.M. of blood glucose values normalised to a baseline level of 5.0 mM shown by dotted horizontal line in response to: •-• 0.7 mg (0.12 μ mol) insulin infused intra-ileally (n = 11), $\blacktriangle - \bigstar 0.7$ mg insulin with 20 mM taurocholate infused intra-ileally (n = 6), and $\nabla - \nabla 0.7$ mg insulin with 20 mM taurocholate infused intra-jejunally (n = 6). Significant reduction from 5.0 mM is denoted by * (P < 0.05); otherwise there was no significant difference (P > 0.05).

Since previous studies have indicated a facilitatory action of co-infusion of bile salts on insulin uptake [41], this was investigated using 20 mM taurocholate in phosphate buffered saline. As shown in Fig. 4c, control experiments in which taurocholate alone was infused into the ileum showed the absence of an effect on the blood glucose level (P = 0.79, Table 3). However, when 0.7 mg insulin co-infused with 20 mM taurocholate (Fig. 3, Fig. 4d, second infusion), there was a dramatic hypoglycaemic response in which the blood glucose concentration was reduced by -3.3 ± 0.9 mM, P = 0.01) with a highly significant cumulative reduction of -18.3 ± 4.2 mM (P = 0.01, Table 3). This hypoglycaemic response was specific to the ileum since no such change was recorded on infusion into the jejunum (Fig. 3, Fig. 4d, first infusion): the cumulative response of $+2.1 \pm 1.2$ mM was non-significant (P = 0.14, Table 3). The facilitatory action on insulin absorption from the ileum also occurred at a much reduced dose of 0.5 mM taurocholate, though with a

reduced response magnitude, and was also evident when prior lavage of the ileum was not undertaken. This suggests that residual bile salts in the ileum may account for the small hypoglycaemic response evident in some insulin experiments (Fig. 4b).



Fig. 4. Representative experiments from 4 different animals showing blood glucose concentration (mM) after the stated intestinal infusions. (a) & (b) 0.7 mg (0.12 μ mol) insulin infused intra-ileally (I51 I.I.) (c) Control intra-ileal infusion of 20 mM Na taurocholate (TCh) showing line of best fit for hyperglycaemic increase with $R^2 = 93.4\%$, $P_{slope} <$ 0.001, after which responsiveness was confirmed by I.A. injection of 50 μ g I51 (d) Coinfusion of 0.7 mg I51 with 20 mM taurocholate, first, intra-jejunally (I51 I.J.) showing line of best fit for hyperglycaemic increase with $R^2 = 92.5\%$, $P_{slope} < 0.001$ and, second, intra-ileally (I51 I.I.).

3.4. Intestinal infusions of cholyl-insulins

Intra-ileal infusions of the B²⁹-Lys-cholyl and B¹-Phe-cholyl conjugates of insulin at a dose equimolar to that of insulin (0.8 mg) dissolved in 1.0 mL of the phosphate or citrate/phosphate buffered saline were then undertaken to determine the extent to which they were absorbed across the ileal mucosa. As shown by the representative experiment in Fig. 5a and normalised mean results in Fig. 6, B²⁹-Lys-cholyl-insulin infused intraileally in 7 animals was without a significant effect on blood glucose levels (P = 0.12, Table 3). In these experiments, the responsiveness of the animal was always confirmed by I.A. injection of conjugate at the end of the experiment.

Table 3

Cumulative changes in blood glucose concentration (mM) after intestinal infusions

Infusate	n	mean \pm S.E.M.	Р
0.7 mg Insulin I.I.	11	$-2.2\pm0.9~\mathrm{mM}$	0.034
20 mM TCh I.I.	6	-0.05 \pm 0.8 mM	0.96
0.7 mg Insulin + TCh I.I.	6	$-18.3\pm4.2~\mathrm{mM}$	0.01
0.7 mg Insulin + TCh I.J.	6	$+2.1\pm1.22~\mathrm{mM}$	0.10
0.8 mg B^{29} -Lys-cholyl-insulin I.I.	7	$-3.3 \pm 1.8 \text{ mM}$	0.12
0.8 mg B^1 -Phe-cholyl-insulin I.I.	7	-11.9 \pm 1.1 mM	0.001
0.8 mg B^1 -Phe-cholyl-insulin + TCh I.I.	6	$+0.4$ \pm 0.9 mM	0.65
0.8 mg B^1 -Phe-cholyl-insulin I.J.	5	$+1.9\pm0.9~\mathrm{mM}$	0.10

Cumulative change in blood glucose concentration as mean \pm S.E.M. with - denoting hypoglycaemia and + denoting hyperglycaemia. I.J. intra-jejunal, I.I. intra-ileal, TCh 20 mM taurocholate. *P* values are for *t*-test against zero.

By contrast, B¹-Phe-cholyl-insulin infusion resulted in a marked hypoglycaemic response which was evident by 30 min after infusion and lasted for 3 h or more (Figs. 5b & 6) and the cumulative hypoglycaemic response of -11.9 ± 1.1 mM for the 7 animals tested was highly significant (P = 0.001, Table 3). This cumulative response may, however, may be an underestimate since, as shown in Fig. 5b, there is an indication that the hypoglycaemic response became evident against a trend to progressive hyperglycaemia. In the experiments, there was no discernible effect of the addition of citrate to the phosphate buffered saline. The dose-dependance of the hypoglycaemic response was further investigated in groups of 5 animals. At a 0.4 mg dose, the cumulative hypoglycaemic response was -2.9 ± 0.7 mM while, at 1.6 mg, it was -6.9 ± 1.0 mM. Both were significantly lower than the response to 0.8 mg (P < 0.01), indicating that 0.8 mg carried in 1.0 mL saline was close to the optimal dose. The process by which B¹-Phe-cholyl-insulin was absorbed from the ileum is indicated by the results of the experiments involving co-infusion of the conjugate with 20 mM taurocholate (Figs. 5c & 6) and the experiments in which the conjugate was infused into the jejunum (Figs. 5d & 6). In each case, the hypoglycaemic response was absent (P > 0.10, Table 3) which is consistent with the uptake of B¹-Phecholyl-insulin by the ileal bile salt transporters.



Fig. 5. Blood glucose levels from 4 different experiments in response (a) intra-ileal infusion of 0.8 mg B²⁹-Lys-cholyl-insulin (CA I51 I.I.) followed by an I.A. dose of 3.1 μ g cholyl-insulin (CA I51 I.A.) (b) intra-ileal infusion of 0.8 mg B¹-Phe-cholyl-insulin (CA I51 I.I.) followed by an I.A. dose of 80 μ g cholyl insulin (CA I51 I.A.) (c) intra-ileal infusion of 0.8 mg B¹-Phe-cholyl-insulin in 20 mM taurocholate (CA I51 I.I.) followed by I.A. dose of 3.5 μ g to test responsiveness (CA I51 I.A.) (d) intra-jejunal infusion of 0.8 mg B¹-Phe-cholyl-insulin (CA I51 I.I.) followed by I.A. dose of 3.5 μ g to test responsiveness (CA I51 I.A.) (d) intra-jejunal infusion of 0.8 mg B¹-Phe-cholyl-insulin (CA I51 I.J.) followed by I.A. dose of 35 μ g to test responsiveness (CA I51 I.A.) (d) intra-jejunal infusion of 0.8 mg B¹-Phe-cholyl-insulin (CA I51 I.J.) followed by I.A. dose of 35 μ g to test responsiveness (CA I51 I.A.) (d) intra-jejunal infusion of 0.8 mg B¹-Phe-cholyl-insulin (CA I51 I.J.) followed by I.A. dose of 35 μ g to test responsiveness (CA I51 I.A.) (d) intra-jejunal infusion of 0.8 mg B¹-Phe-cholyl-insulin (CA I51 I.J.) followed by I.A. dose of 35 μ g to test responsiveness (CA I51 I.A.).

3.5. Histology of small intestinal mucosa

The results shown in Table 3 are based on experiments in which the small intestinal mucosa showed a normal histological appearance in which the mucosa and villi were intact (Fig. 7a). This was also the case when the infusate contained 20 mM taurocholate (Fig. 7b).



Fig. 6. Mean \pm S.E.M. of blood glucose values normalised to a baseline level of 5.0 mM shown by dotted horizontal line in response to: •-• 0.8 mg (0.12 μ mol) B¹-Phecholyl-insulin infused intra-ileally (n = 7), $\blacktriangle - \bigstar 0.8$ mg B¹-Phe-cholyl-insulin with 20 mM taurocholate infused intra-ileally (n = 6), •-• 0.8 mg B¹-Phe-cholyl-insulin infused intrajejunally (n = 5), and $\forall - \forall 0.8$ mg B²⁹-Lys-cholyl-insulin infused intra-ileally (n = 7). Significant reduction from 5.0 mM is denoted by * (P < 0.05); otherwise there was no significant difference (P > 0.05).



Fig. 7. Normal histology of ileal mucosa after experiments involving infusion of (a) 0.8 mg B^1 -Phe-cholyl-insulin in phosphate saline and (b) 0.8 mg B^1 -Phe-cholyl-insulin in phosphate saline and 20 mM taurocholate. The lumen is at the top and the staining was haematoxylin/eosin and alcian blue.

4. Discussion

The major result from the present study is that conjugation of insulin at the free NH_2 group at the B^1 -Phe position with the -COOH group at the C^{24} position of cholic acid to form B¹-Phe-cholyl-insulin promotes absorption from the ileum, while B²⁹-Lys-cholylinsulin showed no indication of being absorbed (Figs. 5a, 5b & 6, Table 3). This result was obtained in experiments in which the animals were shown to maintain a good physiological condition throughout from their well maintained arterial blood pressure and from the integrity of the ileal mucosa (Figs. 7a & b). As a precautionary measure, pyloric ligation was undertaken to prevent the passage of chyme into the duodenum to avoid the release of gastro-intestinal hormones viz. gastrin, cholecystokinin, secretin and gastric inhibitory polypeptide, which have an insulinotropic action [87, 88, 89]. Bilateral vagotomy was also undertaken since the vagus nerves stimulate insulin release [90]. Sometimes, there was the recurring feature of progressive hyperglycaemia which commenced after 3-4 h, particularly in experiments which did not show a hypoglycaemic response viz. the control experiments (Fig. 1), infusion of 20 mM taurocholate alone (Fig. 4c) jejunal infusion experiments (Fig. 4d) and ileal infusion of B²⁹-Lys-cholyl-insulin (Fig. 6). The reason is unlikely to be due to the anaesthetic since this only causes a transient hyperglycaemia which subsides by 30 min post-injection [94], though it may account for the initial settling of the blood glucose concentration seen in many experiments e.g. Fig. 1. The most likely cause of the delayed hyperglycaemia is surgery-induced ACTH release leading to increased systemic cortisol levels. Since cortisol acts genomically [95], its effect in stimulating gluconeogenesis and antagonising insulin-stimulated glucose uptake [96, 97] requires several hours to take effect after which blood glucose levels would increase unless exogenous insulin was administered.

Systemic injections of natural insulin at the standard molar doses of 2 nmol kg^{-1} and 20 nmol kg^{-1} evoked marked hypoglycaemic responses which were especially prolonged at the higher dose (Fig. 2a) and, on a dose per weight basis, are consistent with previously published data in rat [91, 26], dog [29] and man [92]. This was in contrast to the insulin decapeptide and its cholyl conjugate which, even at 500 times the standard insulin molar dose, showed no evidence of biological activity (Fig. 2b) and is inconsistent with the report that the insulin decapeptide possessed 77% of insulin activity [81]. This was based on the promotion of glycogenesis in adipocytes in vitro and highlights the difficulty in relating *in vitro* results to those from the intact animal in which the liver and skeletal muscles have major rôles in glucose uptake. By contrast, both the insulin conjugates, B²⁹-Lys-cholyl-insulin and B¹-Phe-cholyl-insulin, were shown to be biologically active in that, when injected systemically, they caused a hypoglycaemic response which, at the lower standard dose, amounted to some 40% of the insulin response, with a more marked response of extended duration at the higher standard dose (Figs. 2c & d, Table 2). The only previous reports concerning cholyl-insulins relate to systemic injections of B²⁹-Lys-deoxycholyl-insulin which showed a slower onset and longer duration of action than insulin [91] and sub-cutaneous injections of B²⁹-Lys-lithocholyl-insulin which had an enhanced duration of action [93].

For intra-ileal infusions of insulin, there was minimal absorption as shown by an absence of a response or only a small transient hypoglycaemic dip of about 1 mM (Figs. 4a & b)

which is consistent with previous studies (Introduction). This result was unaffected by the inclusion of citrate as a Zn^{2+} chelator in the infusion saline, which excludes hexamer formation as a reason for non-absorption of insulin [83]. There was, however, a very dramatic change when insulin was co-infused with 20 mM taurocholate in that a very marked and prolonged hypoglycaemic response was generated, indicating that appreciable amounts of insulin has been absorbed across the ileal mucosa, though this did not occur with co-infusion into the jejunum (Figs. 3 & 4d, Table 3). This facilitatory action of bile salts on insulin absorption is well documented [29, 34, 41, 53, 54, 55, 56], though the absence of response on jejunal infusion has not previously been noted. The reasons for this difference may stem from the presence in the ileum of Peyer's patches, M cells or bile salt transporters. In the event that the bile salt transporters are indeed involved, this might be explained by the hydrophobic attraction of insulin to the bile salt, which would then be taken up by the bile salt transporters. Irrespective of the actual mechanism, the facilitatory action of residual bile salts may provide the explanation for those cases of ileal infusion of insulin alone in which a small hypoglycaemic response in response was recorded (Fig. 4b).

While intra-ileal infusion of B²⁹-Lys-cholyl-insulin was without effect, there was an unequivocal hypoglycaemic response to infusion of B¹-Phe-cholyl-insulin (Fig. 6, Table 3), which is consistent with the absorption of the B^1 -Phe-cholyl-insulin into the systemic circulation to promote the uptake of glucose by hepatic and muscle cells. While the absence of absorption of B²⁹-Lys-cholyl-insulin is in part disappointing, these experiments are useful for two reasons. The two conjugates are essentially identical chemically and an absence of an effect with the B²⁹-Lys conjugate supports the conclusion that the B¹-Phe conjugate was not being absorbed across the ileal mucosa by passive diffusion or endocytosis. It also confirms that B^1 -Phe-cholyl-insulin was not acting through the release of insulinotropic hormones from the ileum. Since the hypoglycaemic response was abolished by co-infusion with 20 mM taurocholate into the ileum (Figs. 5c & 6) and since the hypoglycaemic response was absent on infusion into the jejunum (Figs. 5d & 6), this would be consistent with absorption of the B^1 -Phe-cholyl-insulin through the bile salt transporters which are specific to the ileum [74]. This is plausible since insulin has an overall negative charge [46], thus providing an anionic substrate for the bile salt transporters which are Na^+ dependent [98].

While rather approximate, there is an indication from a comparison of the intra-ileal and intra-arterial cumulative hypoglycaemic responses (Fig. 5b) that the uptake of B¹-Phe-cholyl-insulin may amount to some 5-10% of the intra-ileal dose. However, this may prove to be an underestimate given that the presumed baseline was sometimes equivocal when the response coincided with the onset the delayed hyperglycaemia *e.g.* Fig. 5b. These experiments were undertaken in normal animals after an overnight fast which was necessary to allow emptying of the gastro-intestinal tract: the alternative of using fed animals would, of necessity, involve additional disturbance to small intestine necessitated by the flushing out of the compacted intestinal contents. During the fast, our animals did have access to a sucrose drink which may be surmised to cause endogenous insulin release in order to regulate their blood glucose levels. The fact that B¹-Phe-cholyl-insulin did cause sustained hypoglycaemic responses from normoglycaemic levels in our animals (Fig. 6) may be taken as an encouraging sign for the next stage which would be to determine its effectiveness against uncontrolled hyperglycaemia in diabetic animals without endogenous insulin. Subsequently, it would then need to be established that the result is transferable across the species barrier with the ultimate challenge being in human subjects. In establishing that B¹-Phe-cholyl-insulin was taken up by the ileal bile salt transporters, the uptake was shown to be inhibited by co-infusion of 20 mM taurocholate (Fig. 6), which introduces a potential complication in that, in the normally functioning small intestine, endogenous bile salts would reduce the uptake of B^1 -Phe-cholyl-insulin due to competition for sites on the bile salt transporters. However, the rat is unusual in that it releases bile continuously into the duodenum due to the absence of a gall bladder whereas, in man, bile is stored in the gall bladder and is released upon entry of lipids into the duodenum to cause CCK release which is the main effector of gall bladder contraction [99]. This means that delivery of cholyl-insulin in protective capsules prior to a meal could still be a feasible means of promoting absorption by the ileal mucosa. At present, there are 13 initiatives underway using encapsulated insulin, insulin nanoparticles and B^{29} -PEG insulin to enhance the uptake of natural insulin by the intestinal mucosa [38]. Given the toxicity issues and the tendency for initiatives to be abandoned at an early stage, the outlook for an oral insulin formulation is by no means certain [42]. So, it may be timely to consider a new approach in the form of a cholyl-insulin formulation by which absorption is achieved by secondary active transport rather than by passive diffusion and is not dependent upon protease inhibitors or permeation enhancers (Table 1). This may constitute a more productive avenue for further development.

References

- 1. Banting FG, Best CH, Collip JB, Campbell WR & Fletcher AA (1922) Pancreatic extracts in the treatment of diabetes mellitus. The Canadian Medical Association Journal 12:141-146
- 2. The Diabetes Control and Complications Trial Research Group (2000) Retinopathy and nephropathy in patients with type 1 diabetes four years after a trial of intensive therapy. New England Journal of Medicine 342:381-389
- 3. Kumar PJ & Clark ML (1998) Clinical Medicine 4th Ed. WB Saunders, London
- 4. Burkoth TL, Bellhouse BJ, Hewson G, Longridge DJ, Muddle AG & Sarphie DF (1999) Transdermal and transmucosal powdered drug delivery. Critical Reviews in Therapeutic Drug Carrier Systems 16:331-384
- 5. Skyler JS, Cefalu WT, Kourides IA, Landschultz WH, Balagtas CC, Cheng S-L, Gelfand RA (2001) Efficacy of inhaled human insulin in type 1 diabetes mellitus: a randomised proof-of-concept study. Lancet 357:331-335.
- 6. Shapiro AMJ, Lakey JRT, Ryan EA, Korbutt GS, Toth E, Warnock GL, Kneteman NM & Rajotte RV (2000) Islet transplantation in seven patients with type 1 diabetes mellitus using a glucocorticoid-free immunosuppressive regimen. New England Journal of Medicine 343:230-238
- 7. Dudley HW (1923) XLII. The purification of insulin and some of its properties. Biochemical Journal 17:376-390

- 8. Scott DA (1925) The action of trypsin on insulin. Journal of Biological Chemistry 63:641-651
- Trenktrog T, Müller BW & Seifert J (1995) In vitro-investigation into the enhancement of intestinal peptide absorption by emulsion systems. European Journal of Pharmacology & Biochemistry 41:284-290
- 10. Witzemann EJ & Livshis L (1923) The action of proteolytic enzymes upon insulin. Journal of Biological Chemistry 57:425-435
- 11. Arbit, E Kidron M (2009) Oral insulin: the rationale for this approach and current developments. Journal of Diabetes Science & Technology 3:562-567
- 12. Amino Y, Kawada K, Toi K, Kumashiro I & Fukushima K (1988) Phenyalanine derivatives enahancing intestinal absorption of insulin in mice. Chemical & Pharmaceutical Bulletin 36:4426-4434
- 13. Asada H, Douen T, Waki M, Adachi S, Fujita T, Yamamoto A & Muranishi S (1995) Absorption characteristics of chemically-modified insulin derivatives with various fatty acids in the small and large intestine. Journal of Pharmaceutical Sciences 84:682-687
- 14. Calceti P, Salmaso S, Walker G & Bernkop-Schnürch A (2004) Development and in vivo evaluation of an oral insulin-PEG delivery system. European Journal of Pharmaceutical Sciences 22:315-323
- 15. Chalasani KB, Russell-Jones GJ, Yandrapu SK, Diwan PV & Jain SK (2007) A novel vitamin B_{12} -nanosphere conjugate carrier system for peroral delivery of insulin. Journal of Controlled Release 117:421-429
- Dekel Y, Glucksam Y & Margalit R (2010) Novel fibrillar insulin formulations for oral administration: formulation and in vivo studies in diabetic mice. Journal of Controlled Release 143:128-135
- 17. Engel RH, Riggi SJ & Fahrenbach MJ (1968) Insulin: intestinal absorption as waterin-oil-in-water emulsions. Nature 219:856-857
- 18. Fasano A & Uzzau S (1997) Modulation of intestinal tight junctions by zonula occludens toxin permits enteral administration of insulin and other macromolecules in an animal model. Journal of Clinical Investigation 99:1158-1164
- 19. Mesiha MS, Ponnapula S & Plakogiannis F (2002) Oral absorption of insulin encapsulated in artificial chyles of bile salts, palmitic acid and α -tocopherol dispersions. International Journal of Pharmaceutics 249:1-5
- 20. Morishita I, Morishita I, Takayama K, Machida Y & Nagai T (1993) Site-dependent effect of aprotinin, sodium caprate, Na₂EDTA and sodium glycocholate on intestinal absorption of insulin. Biological & Pharmaceutical Bulletin 16:68-72
- 21. Morishita M, Aoki Y, Sakagami M, Nagai T & Takayama1 K (2004) In situ ileal absorption of insulin in rats: effects of hyaluronidase pretreatment diminishing the mucous/glycocalyx layers. Pharmaceutical Research 21:309-316

- 22. Morishita M, Gotoa T, Nakamura K, Lowmanb AM, Takayama K & Peppas NA (2006) Novel oral insulin delivery systems based on complexation polymer hydrogels: single and multiple administration studies in type 1 and 2 diabetic rats. Journal of Controlled Release 110:587594
- 23. Morishita M, Kamei N, Ehara J, Isowa K & Takayama K (2007) A novel approach using functional peptides for efficient intestinal absorption of insulin. Journal of Controlled Release 118:177184
- 24. Niu M, Lua Y, Hovgaard L, Guan P, Tan Y, Lian R, Qi J& Wu W (2012) Hypoglycemic activity and oral bioavailability of insulin-loaded liposomes containing bile salts in rats: the effect of cholate type, particle size and administered dose. European Journal of Pharmaceutics and Biopharmaceutics 81:265272
- 25. Rekha MR & Sharma CP (2009) Synthesis and evaluation of lauryl succinyl chitosan particles towards oral insulin delivery and absorption. Journal of Controlled Release 135:144151
- 26. Roberts, PA, Burney, JD, Black KW. & Zaloga GP (1999) Effect of chain length on absorption of biologically active peptides from the gastrointestinal tract. Digestion 60:332-337
- 27. Rodier-Bruant C, Vaxman F, Lambert A, Wagner D, Coumaros G, Vaultier J-P, Koenig M & Grenier J-F (1991) Étude de l'absorption intestinale de l'insuline chez le chien grâce à une nouvelle capsule de largage télémétrique. Gastroentérologie Clinique et Biologique 15:187-193
- 28. Sajeesh S, Bouchemal K, Marsaud V, Vauthier C, & Sharma CP (2010) Cyclodextrin complexed insulin encapsulated hydrogel microparticles: An oral delivery system for insulin. Journal of Controlled Release 147:377384
- 29. Scott-Moncrieff JC, Shao Z & Mitra AK (1994) Enhancement of intestinal insulin absorption by bile salt-fatty acid mixed micelles in dogs. Journal of Pharmaceutical Sciences 83:1465-1469
- 30. Shichiri M, Shimizu Y, Yoshida Y, Kawamori R, Fukuchi M, Shigeta Y & Abe H (1974) Enteral absorption of water-in-oil-in-water insulin emulsions in rabbits. Diabetologia 10:317-321
- 31. Taverner A,Dondi R, Almansour K, Laurent F, Owens S-E, Eggleston IM, Fotaki N & Mrsny RJ (2015) Enhanced paracellular transport of insulin can be achieved via transient induction of myosin light chain phosphorylation. Journal of Controlled Release 210:189-197
- 32. Touitou E, Donbrow M & Rubinstein A (1980) Effective intestinal absorption of insulin in diabetic rats using a new formulation approach. Journal of Pharmacy & Pharmacology 32:108-110
- 33. Yamamoto A, Taniguchi T, Rikyuu K, Tsuji T, Fujita T, Murakami M & Muranishi S (1994) Effects of various protease inhibitors on the intestinal absorption and degradation of insulin in rats. Pharmaceutical Research 11:1496-1500

- 34. Ziv E, Lior O & Kidron M (1987) Absorption of protein via the intestinal wall. Biochemical Pharmacology 36:1035-1039
- 35. Speth RN & Chistian HJ (1963) Studies on the absorption of insulin from the gastrointestinal tract of the rabbit. Diabetes 12:243-248
- 36. Al-Achi A & Greenwood R (1994) Human insulin absorption from the intestine in diabetic rats. Drug Development and Industrial Pharmacy 20:2333-2339
- 37. Eldor R, Arbit E, Corcos A & Kidron M (2013) Glucose-reducing effect of the ormd-0801 oral insulin preparation in patients with uncontrolled type 1 diabetes: a pilot study. PLOS ONE 8:e59524
- 38. Zijlstra E, Heinemann L & Plum-Mörschel L (2014) Oral insulin reloaded: a structured approach. Journal of Diabetes Science & Technology 8:458-465
- Anderson, JM & Van Itallie CM (1995) Tight junctions and the molecular basis for regulation of paracellular permeability. American Journal of Physiology (Gastrointestinal & Liver Physiology) 32:G467-G475
- 40. Trier JS (1991) Structure and function of intestinal M cells. Gastroenterology Clinics of North America 20:531-547
- 41. Bendayan M, Ziv E, Ben-Sasson R, Bar-On H & Kidron M (1990) Morphocytochemical and biochemical evidence for insulin absorption by the rat ileal epithelium. Diabetologia 33:197-204
- 42. Fonte P, Arújo F, Reis S & Sarmento B (2013) Oral insulin delivery: how far are we? Journal of Diabetes Science & Technology 7:520-531
- 43. Nielsen EJB, Yoshida S, Kamei N, Iwamae R, Khafagy E-S, Olsen J, Rahbek UL, Pedersen BL, Takayama K, & Takeda-Morishita M (2014) *In vivo* proof of concept of oral insulin delivery based on a co-administration strategy with the cell-penetrating peptide penetratin. Journal of Controlled Release 189:1924
- 44. Kamei N, Morishita M, Kanayama Y, Hasegawa K, Nishimura N, Hayashinaka E , Wada Y, Watanabe Y & Takayama K (2010)Molecular imaging analysis of intestinal insulin absorption boosted by cell-penetrating peptides by using positron emission tomography. Journal of Controlled Release 146:16-22.
- 45. Niu M, Tan Y,Guan P, Hovgaard L, Lu Y, Qi J, Lian R, Li X & Wu W (2014) Enhanced oral absorption of insulin-loaded liposomes containing bile salts: a mechanistic study. International Journal of Pharmaceutics 460:119-130.
- 46. Ritschel WA (1991) Microemulsions for improved peptide absorption from gastrointestinal tract. Methods & Findings in Experimental & Clinical Pharmacology 13:205-220
- 47. Aprahamian M, Michel C, Humbert W, Devissaguet J-P & Damgé C (1987) Transmucosal passage of polyalkylcyanoacrylate nanocapsules as a new drug carrier in the small intestine. Biology of the Cell 61:69-76

- 48. Chuang E-Y, Lin K-J, Su F-Y, Mi F-L, Maiti B, Chen C-T, Wey S-P, Yen T-C, Juang J-H & Sung H-W (2013) Noninvasive imaging oral absorption of insulin delivered by nanoparticles and its stimulated glucose utilization in controlling postprandial hyperglycemia during OGTT in diabetic rats. Journal of Controlled Release 172:513522
- 49. Liu M,Zhang J,Zhu X, Shan W, Li L, Zhong J, Zhang Z & Y Huang Y (2015) Efficient mucus permeation and tight junction opening by dissociable mucus-inert agent coated trimethyl chitosan nanoparticles for oral insulin delivery Journal of Controlled Release (2015),
- 50. Lowe PJ & Temple CS (1994) Calcitonin and insulin in isobutylcyanoacrylate nanocapsules: protection against proteases and effect on intestinal absorption in rats. Journal of Pharmacy & Pharmacology 46:547-552
- 51. Damgé C, Maincent P & Ubrich N (2007) Oral delivery of insulin associated to polymeric nanoparticles in diabetic rats. Journal of Controlled Release 117:163-170
- 52. Jeffries GH (1967) Gastric secretion of intrinsic factor. In: Code CF (Ed) Handbook of Physiology- Alimentary Canal II pp. 919-924 American Physiological Society, Washington
- 53. Kidron M, Bar-On H, Berry EM & Ziv E (1982). The absorption of insulin from various regions of the rat intestine. Life Sciences 31:2837-2841
- 54. New RRC (1996) Pharmaceutical compositions containing a bile salt and a buffer for increased bioavailability of an active compound. International Patent Application WO 96/06635 The Patent Office, Newport, Wales
- 55. Bendayan M, Gingras D, Ben-Sasson R, Bar-On H & Kidron M (1994) Biochemical and morpho-cytochemical evidence for the intestinal absorption of insulin in control and diabetic rats. Comparison between the effectiveness of duodenal and colon mucosa. Diabetologia 37:119-126
- 56. Schilling RJ & Mitra AK (1990) Intestinal mucosal transport of insulin. International Journal of Pharmaceutics 62:53-64
- 57. Jederström G, Andersson A, Gråsjö J & Sjöholm I (2004) Formulating insulin for oral administration: preparation of hyaluronan-insulin complex. Pharmaceutical Research 21:2040-2047
- 58. Jederström G, Gråsjö J, Nordin A, Sjöholm & Andersson A (2005) Blood glucoselowering activity of a hyaluronan-insulin complex after oral administration to rats with diabetes. Diabetes Technology & Therapeutics 7:948-957
- 59. Li J, Wang Y, Han L, Sun X, Yu H & Yu Y (2012) Time-action profile of an oral enteric insulin formulation in healthy Chinese volunteers. Clinical Therapeutics 34:2333-2338
- 60. Lin S-Y & Kawashima Y (1987) Drug release from tablets containing cellulose acetate phthalate as an additive or enteric-coating material. Pharmaceutical Research 4:70-74

- 61. Maharaj I, Nairn JG & Campbell JB (1984) Simple rapid method for the preparation of enteric-coated microspheres. Journal of Pharmaceutical Sciences 73:39-42
- 62. Takenaka H, Kawashima Y & Lin S-Y (1980) Preparation of enteric-coated microcapsules for tableting by spray-drying techniques and *in vitro* simulation of drug release from the tablet in GI tract. Journal of Pharmaceutical Sciences 69:1388-1392
- 63. Sonaje K, Chen Y-J, Chen H-L, Wey S-P, Juang J-H, Nguyen H-N, Hsu C-W, Lin K-J & Sung H-W (2010) Enteric-coated capsules filled with freeze-dried chitosan/poly(γ -glutamic acid) nanoparticles for oral insulin delivery. Biomaterials 31:3384-3394
- 64. Suzuki A, Morishita M, Kajita M, Takayama K, Isowa K, Chiba Y, Tokiwa S & Nagai T (1998) Enhanced colonic and rectal absorption of insulin using a multiple emulsion containing eicosapentaenoic acid and docosahexaenoic acid. Journal of Pharmaceutical Sciences 87:1196-1202
- 65. Kapitza C, Zijlstra E, Heinmann L, Castelli MC, Riley G & Heise H (2010) Oral insulin: a comparison with subcutaneous regular human insulin in patients with type 2 diabetes mellitus. Diabetes Care 33:1288-1290
- 66. Elsayed A, Al-Remawi H, Farouk A & Badwan A (2010) Insulin-chitosan polyelectrolyte-anocomplexes: preparation, characterization and stabilization of insulin. Sudan Journal of Medical Sciences 5:99-110
- 67. Damgé C, Vranckx H, Balschmidt P & Couvreur P (1997) Poly(alky cyanoacrylate) nanospheres for oral administration of insulin. Journal of Pharmaceutical Science 86:1403-1409
- 68. Michel C, Aprahamian M, Defontaine L, Couvreur P & Damagé C (1991) The effect of site of administration in the gastrointestinal tract on the absorption of insulin from nanocapsules in diabetic rats. Journal of Pharmacy & Pharmacology 43:1-5
- 69. Cui F, Shi K, Zhang L, Tao A & Kawashima Y (2006) Biodegradable nanoparticles loaded with insulinphospholipid complex for oral delivery: Preparation, in vitro characterization and in vivo evaluation. Journal of Controlled Release 114:242250
- 70. Xiong XY, Li YP, Li ZL, Zhou CL, Tamb KC, Liu ZY & Xie GX (2007) Vesicles from Pluronic/poly(lactic acid) block copolymers as new carriers for oral insulin delivery. Journal of Controlled Release 120:1117
- 71. Mathiowitz E, Jacob JS, Jong YS, Carino GP, Chickering DE, Chatturvedi P, Santos CA, Vijayaraghavan K, Montgomery S, Bassett M & Morrell C (1997) Biologically erodable microspheres as potential oral drug delivery systems. Nature 386:410-414
- 72. Thompson CJ, Tetley L, Uchegbu IF & Cheng WP (2009) The complexation between novel comb shaped amphiphilic polyallylamine and insulin-Towards oral insulin delivery. International Journal of Pharmaceutics 376:46-55
- 73. Muranishi S, Murakami M, Hashidzume M, Yamada K, Tajima S & Kiso Y (1992) Trials of lipid modification of peptide hormones for intestinal delivery. Journal of Controlled Release 19:179-188

- 74. Baker RD & Searle GW (1960) Bile salt absorption at various levels of the rat small intestine. Proceedings of the Society for Experimental Biology & Medicine 105:521-523
- 75. Kramer W, Wess G, Neckermann G, Schubert G, Fink J, Girbig F, Gutjahr U, Kowalewski S, Baringhaus K-H, Boger G, Enhsen A, Falk E, Friedrich M, Glombik H, Hoffmann A, Pittius C & Urman M et al. (1994) Intestinal absorption of peptides by coupling to bile acids. Journal of Biological Chemistry 269:10621-10627
- 76. Swaan PW, Hillgren KM, Szoka FC & Øie S (1997) Enhanced transepithelial transport of peptides by conjugation to cholic acid. Bioconjugate Chemistry 8:520-525
- 77. Stephan ZF, Yurachek EC, Sharif R, Wasvary JM, Steele RE & Howes C (1992) Reduction of cardiovascular and thyroxine-suppressing activities by L-T₃ by liver targeting with cholic acid. Biochemical Pharmacology 43:1969-1974
- 78. Byun Y & Lee Y-K (2001) Amphiphilic polysaccharide derivatives. United States Patent 6245753 United States Patent & Trademark Office, Alexandria USA
- Wheeler S, McGinn BJ, Lucas ML & Morrison JD (2002) Absorption of biologically active peptide hormones from the small intestine of rat. Acta Physiologica Scandinavica 176, 203-213
- 80. McHarg S, Morton JS, McGinn BJ, Yasin M, & Morrison, JD (2004) Absorption of the cholic acid-conjugated peptide hormone cholylsecretin from the rat ileum in vivo. Acta Physiologica Scandinavica 181:23-34
- Prozorovskiy VN, Maksimova EM, Alekseeva AE, Grebenschikova OG, Abakumova OY, Kutsenko NG, Ivanov AS, Kniazhev VN & Archakov AI (1999) Synthetic insulin fragment with insulin-like biological activity. Biochemistry & Molecular Biology International 47:957-963
- 82. Lindsay DG & Shall S (1969) Acetoacetylation of insulin. Biochemical Journal 115:587-595
- 83. Baker EN, Blundell TL, Cutfield JF, Cutfield SM, Dodson EJ, Dodson GG, Crowfoot Hodgkin DM, Hubbard RE, Isaacs NW, Reynolds CD, Sakabe K, Sakabe N, & Vijayan NM (1988) The structure of 2Zn pig insulin crystals at 1.5 Å resolution. Philosophical Transactions of the Royal Society of London Series B Biological Sciences 319:369-456
- 84. Norman A (1954) On the conjugation of bile acids in the rat. Acta Physiologica Scandinavica 32:1-10
- 85. Morrison JD (2012). Prolonged stimulation of pancreatic serous secretions by bile and sodium taurocholate in anaesthetized rats. Journal of Physiology & Biochemistry 68:503-520
- 86. Smith LF (1966) Species variation in the amino acid sequence of insulin. American Journal of Medicine 40:662-666
- 87. Dupré J, Rojas, L, White JJ, Unger RH & Beck JC (1966) Effects of secretin on insulin and glucagon in portal and peripheral blood in man. Lancet 288:26-27

- 88. Dupré J, Ross SA, Watson D & Brown JC (1973) Stimulation of insulin secretion by gastric inhibitory polypeptide in man. Journal of Clinical Endocrinology & Metabolism 37:826-828
- 89. Unger RH, Ketterer J, Dupré J & Eisentraut AM (1967) The effects of secretin, pancreozymin and gastrin on insulin and glucagon secretion in anaesthetized dogs. Journal of Clinical Investigation 46:630-645
- 90. Daniel PM & Henderson JR (1967). The effect of vagal stimulation on plasma insulin and glucose levels in baboons. Journal of Physiology 192:317-327
- 91. Lee S, Kim K, Kumar TS, Lee J, Kim SK, Lee DY, Lee Y & Byun Y (2005) Synthetic and biological properties of insulin-deoxycholic acid chemical conjugates. Bioconjugate Chemistry 16:615-620
- 92. Bell GH, Emslie-Smith D & Paterson CR (1976) Textbook of Physiology and Biochemistry 9th Ed. Churchill-Livingstone, Edinburgh
- 93. Jonassen I, Havelund S, Ribel U, Plum A, Loftager M, Hoeg-Jensen T, Volund A & Markussen J (2006) Biochemical and physiological properties of a novel series of long-acting insulin analogs obtained by acylation with cholic acid derivatives. Pharmaceutical Research 23:49-55
- 94. Pénicaud L, Ferre P, Kande J, Letrque A, Issad T & Girard J (1987). Effect of anaesthesia on glucose production and utilization in rats. American Journal of Physiology (Endocrinology & Metabolism) 252:E365-369
- 95. Berne RM, Levy MN, Koeppen BM & Stanton BA (1998) Physiology
 4^{th} Ed. Mosby, St Louis
- 96. Desborough JP (2000) The stress response to trauma and surgery. British Journal of Anaesthesia 85:109-117
- 97. McCowan KC, Malhotra A & Bistrian BR (2001) Stress-induced hyperglycaemia. Critical Care Clinics 17:107-124
- Playoust MR & Isselbacher KJ (1964) Studies on the transport and metabolism of conjugated bile salts by intestinal mucosa. Journal of Clinical Investigation 43:467-476
- Davenport HW (1977) Physiology of the Digestive Tract 4th Ed. Year Book Medical Publishers Inc., Chicago