Bekim Osmani*, Gabriela Gerganova and Bert Müller

Biomimetic nanostructures for the silicone-biosystem interface: tuning oxygen-plasma treatments of polydimethylsiloxane

DOI 10.1515/ejnm-2017-0002
Received February 2, 2017; accepted March 2, 2017

Abstract: Polydimethylsiloxanes (PDMS) have drawn attention because of their applicability in medical implants, soft robotics and microfluidic devices. This article examines the formation of dedicated nanostructures on liquid submicrometer PDMS films when exposed to oxygen-plasma treatment. We show that by using a vinyl-terminated PDMS prepolymer with a molecular weight of 800 g/mol, one can bypass the need of solvent, copolymer, or catalyst to fabricate wrinkled films. The amplitude and periodicity of the wrinkles is tuned varying the thickness of the PDMS film between 150 and 600 nm. The duration of the plasma treatment and the oxygen pressure determine the surface morphology. The amplitude was found between 30 and 300 nm with periodicities ranging from 500 to 2800 nm. Atomic force microscopy was used to measure film thickness, amplitude and wrinkle periodicity. The hydrophobic recovery of the nanostructured PDMS surface, as assessed by dynamic contact angle measurements, scales with nanostructure’s fineness, associated with an improved bio compatibility. The mechanical properties were extracted out of 10,000 nanoindentations on 50 × 50-µm² spots. The mechanical mapping with sub-micrometer resolution reveals elastic properties according to the film morphology. Finally, we tailored the mechanical properties of a 590 ± 120-nm-thin silicone film to the elastic modulus of several MPa, as required for dielectric elastomer actuators, to be used as artificial muscles for incontinence treatments.

Keywords: dielectric elastomer actuators; dynamic contact angle measurements on PDMS; local mechanical properties of thin polymer films; nanometer-thin polymer films; oxygen-plasma-tuned wrinkles.

Introduction

Polydimethylsiloxane (PDMS) elastomers are inexpensive, flexible, biocompatible, optically transparent materials and their manifold fabrication techniques, such as spin coating, electrospraying, molecular beam deposition, 3D printing and molding, have led to a numerous applications (1–6). They are widely used in soft robotics, flexible electronics, microfluidic devices, medical implants, cell culture substrate and dielectric elastomer actuators, as shown in Figure 1 (3, 7–14). Its native hydrophobic surface exhibits a water contact angle of 120° ± 4° and is mainly determined by the CH₃ groups. It can easily become hydrophilic by the introduction of silanol functional groups on the PDMS surface via oxygen-plasma or ultraviolet/ozone treatments (15–18). The hydrophilicity decays with time, if stored in air, due to the migration of the smaller polymer chains from the bulk to the surface, reorientation of the polar groups and condensation of hydroxyl groups (18). The oxygen-plasma treatment forms a silica-like surface layer and its thickness increases with treatment duration and RF plasma power (19). The oxygen plasma does not only change the wettability but also alters the surface topography (20). Wavy patterns arise due to the mismatch of the thermal expansion coefficient of the formed silica-like layer and the bulk PDMS. The heating originates from the plasma itself and causes the PDMS layer to expand. Upon cooling, the bulk PDMS shrinks much more than the stiff silica-like film and exerts a compressive stress on the stiff film on top.

This stress is released by forming a wrinkling pattern on the elastomeric substrate. For thermally cross-linked PDMS films, the wrinkles can be tailored in amplitude and periodicity (21–23). It has been shown that nanostructures of plasma-treated submicrometer-thin liquid films of dissolved PDMS prepolymer with a molecular weight of 139,000 g/mol can vary with the thickness of...
the film (24). In addition, many communications report on the estimated elastic modulus for the silica-like surface layer, which was found to be between 4 MPa and 1.5 GPa (15, 19).

The interface between man-made material and the human body is critical for the functionality of a medical implant. In general, the body recognizes the implant as foreign body resulting in encapsulation. Several researchers have demonstrated, however, that nanostructures similar to the hydroxyapatite crystallites promote protein adsorption and can reduce the inflammatory reactions (25–29). Nanostructures on plasma-treated polymer polyetheretherketone can even support osteogenic differentiation of human mesenchymal stem cells in vitro (30, 31). Another key parameter that affects cell behavior is the substrate elasticity (32). Consequently, the present study on tailoring the surface morphology and elasticity tuning the plasma treatment is an essential step to realize next-generation silicone implants.

Here, we show that using a vinyl-terminated PDMS prepolymer with a molecular weight of 800 g/mol, we can bypass the need of a solvent or a cross-linking agent to fabricate PDMS films in the nanometer range. The amplitude and the periodicity of the wrinkles were tuned decreasing the film thickness, adapting the treatment duration and the oxygen pressure. Finally, we have extracted the mechanical properties of a plasma-treated PDMS film with a submicrometer resolution and showed that the average elastic modulus can be set to a few MPa, as required for low-voltage dielectric elastomer actuators as proposed for artificial muscles (33).

Materials and methods

Preparation of PDMS films

Vinyl-terminated PDMS (V05, Gelest, Inc., Morrisville, PA, USA) with a number average molecular weight of 800 g/mol and a kinematic viscosity of 6±2 cSt was spun (WS-400B-6NPP/LITE/AS, Laurell Technologies Corporation, North Wales, PA, USA) onto 2-inch silicon wafers as supplied (SIEGERT WAFER GmbH, Germany). The thickness of the PDMS films was determined by scanning an edge using atomic force microscopy (AFM) in tapping mode as shown in Figure 2.

The PDMS films were prepared by pre-selected rotational speeds and spin durations to realize a variety of film thicknesses. The film thickness of 590±120 nm was found at a speed of 3000 rpm applied for 2 min. Increasing the speed to 6000 rpm and applying the same duration, we have found a thickness of 350±50 nm. The thickness was reduced to 150±20 nm using a speed of 7000 rpm for 4 min.

Oxygen-plasma treatment of PDMS films

The specimens were oxygen-plasma treated using a power of 200 W for durations of 18, 36, 72 and 144 s and a frequency of 40 kHz (PICO System, Diener Electronics, Ebhausen, Germany). The oxygen partial pressure (Carbagas, Gümligen, Switzerland) was controlled varying the oxygen flow rate from 15 to 40 sccm. The application of an oxygen-plasma treatment alters the surface topography as schematically shown in Figure 3.

Dynamic contact angle measurements

The specimens were aged for a period of 180 days prior to contact angle measurements to study the hydrophobic recovery of the nanometer-thin films. They were placed on a tiltable stage of a contact angle goniometry device (OCA 15 EC, Version 2.1, DataPhysics...
The elastic modulus of the oxygen-plasma treated PDMS films was assessed by AFM nanoindentation (NI) techniques (FlexAFM C3000, Nanosurf AG, Switzerland). For this purpose, 10,000 NIs were applied on 50 µm × 50 µm spots using a spherical tip with a radius of 522 ± 2 nm (B500_FMR, Nanotools GmbH, Germany). The nominal spring constant of the AFM cantilever was found to be 1.9 ± 0.1 N/m as determined by the Sader method (34). During a single NI measurement, the sample was moved toward the AFM tip until the previously defined force of F = 200 nN was achieved. The additional information of the z-piezo allowed to extract the indentation depth and calculate the mean elastic modulus E.

$E = \frac{4F \cdot d}{A \cdot (1-\nu^2)}$
modulus $E$ using the Hertz contact model, which is implemented in the FLEX-ANA® software (Automated Nanomechanical Analysis, Nanosurf AG, Switzerland). Potential substrate effects were neglected since the indentation depths were less than 20% of the total film thickness.

AFM imaging

AFM images were acquired by raster-scanning a soft AFM-probe with a radius smaller than 10 nm (Tap190Al-G probe, NanoAndMore GmbH, Wetzlar, Germany) in tapping mode (vibration amplitude 2.0 V, set point 60%) using a FlexAFM System (Nanosurf AG, Liestal, Switzerland). A total of 512 lines at a speed of 1 s per line were acquired for each image. The raw data were leveled by subtracting a mean plane and removing a polynomial background of the first degree. Root-mean-square (RMS) roughness values were calculated using 2D fast Fourier transform (2D FFT) of the related AFM image. The periodicity $\lambda$ and the amplitude $A$ decrease with film thickness.

We show in Figure 6 dynamic contact angle measurements and AFM images of surfaces of 350 ± 50 nm PDMS films, which were oxygen-plasma treated ($P_{\text{plasma}} = 200$ W, $t_{\text{plasma}} = 60$ s, $p_{\text{ox}} = 45$ Pa, $T_s = 25^\circ\text{C}$) at oxygen pressures from $p_{\text{ox}} = 18$ to $p_{\text{ox}} = 45$ Pa. The amplitude $A$, as extracted out the height distribution diagram and the periodicity/wavelength $\lambda$ of the wrinkles are summarized in Table 1. It is found that the periodicity $\lambda$ and the amplitude $A$ increase at lower oxygen pressures $p_{\text{ox}}$.

PDMS films with a thickness of 350 ± 50 nm were oxygen-plasma treated ($P_{\text{plasma}} = 200$ W, $t_{\text{plasma}} = 60$ s, $p_{\text{ox}} = 45$ Pa, $T_s = 25^\circ\text{C}$) by varying the treatment duration from 18 to 144 s are shown in Figure 7. The amplitude $A$, as extracted out the height

---

**Results**

AFM scans and dynamic contact angle measurements of the oxygen-plasma treated PDMS films ($P_{\text{plasma}} = 200$ W, $t_{\text{plasma}} = 60$ s, $p_{\text{ox}} = 45$ Pa, $T_s = 25^\circ\text{C}$) are shown in Figure 5. The amplitude $A$, as extracted out the height distribution diagram and the periodicity/wavelength $\lambda$ of the wrinkles are summarized in Table 1. The periodicity $\lambda$ is calculated using 2D fast Fourier transform (2D FFT) of the related AFM image. The periodicity $\lambda$ and the amplitude $A$ decrease with film thickness.

We show in Figure 6 dynamic contact angle measurements and AFM images of surfaces of 350 ± 50 nm PDMS films, which were oxygen-plasma treated ($P_{\text{plasma}} = 200$ W, $t_{\text{plasma}} = 60$ s, $T_s = 25^\circ\text{C}$) at oxygen pressures from $p_{\text{ox}} = 18$ to $p_{\text{ox}} = 45$ Pa. The amplitude $A$, as extracted out the height distribution diagram and the periodicity/wavelength $\lambda$ of the wrinkles are summarized in Table 1. It is found that the periodicity $\lambda$ and the amplitude $A$ increase at lower oxygen pressures $p_{\text{ox}}$.

PDMS films with a thickness of 350 ± 50 nm were oxygen-plasma treated ($P_{\text{plasma}} = 200$ W, $t_{\text{plasma}} = 60$ s, $p_{\text{ox}} = 45$ Pa, $T_s = 25^\circ\text{C}$) by varying the treatment duration from 18 to 144 s are shown in Figure 7. The amplitude $A$, as extracted out the height

---

**Figure 5:** AFM scans and dynamic contact angle measurements of PDMS films with varying film thicknesses $h_{\text{PDMS}}$.

The amplitude $A$ and periodicity $\lambda$ of the wrinkles show a positive correlation with the film thickness. The contact angle $\theta$ decreased with decrement in film thickness from $107^\circ ± 1^\circ$ to $96^\circ ± 1^\circ$ and the hysteresis $\Delta \theta$ shows a tendency towards smaller values.

**Table 1:** Contact angle, periodicity and amplitude of plasma-treated PDMS films ($P_{\text{plasma}} = 200$ W, $t_{\text{plasma}} = 60$ s, $p_{\text{ox}} = 45$ Pa, $T_s = 25^\circ\text{C}$) for selected film thicknesses.

<table>
<thead>
<tr>
<th>Film thickness $h_{\text{PDMS}}$, nm</th>
<th>Contact angle $\theta$, deg</th>
<th>Hysteresis $\Delta \theta$ at $\alpha = 90^\circ$, deg</th>
<th>Periodicity of the wrinkles $\lambda$, nm</th>
<th>Amplitude $A$, nm</th>
<th>Ratio amplitude to film thickness $A/h_{\text{PDMS}}$</th>
</tr>
</thead>
<tbody>
<tr>
<td>590 ± 120</td>
<td>107 ± 1</td>
<td>11 ± 1</td>
<td>2800 ± 200</td>
<td>&gt;200</td>
<td>&gt;1/3</td>
</tr>
<tr>
<td>350 ± 50</td>
<td>99 ± 1</td>
<td>10 ± 1</td>
<td>1100 ± 100</td>
<td>&gt;90</td>
<td>&gt;1/4</td>
</tr>
<tr>
<td>150 ± 20</td>
<td>96 ± 1</td>
<td>9 ± 1</td>
<td>500 ± 100</td>
<td>&gt;30</td>
<td>&gt;1/5</td>
</tr>
</tbody>
</table>
distribution diagram, and the periodicity/wavelength $\lambda$ of the wrinkles are listed in Table 3. The periodicity $\lambda$ was calculated using 2D fast Fourier transform (2D FFT) of the related AFM images and are found to remain constant at $1100 \pm 100$ nm for the selected conditions.

A PDMS film with a thickness of $590 \pm 120$ nm was plasma-treated at an RF power $P_{\text{plasma}} = 200$ W for a total duration of $t_{\text{plasma}} = 60$ s. The mechanical mapping with submicrometer resolution, shown in Figure 8, reveals topology-dependent elastic properties. It exhibits elastic moduli of $1.8 \pm 0.6$ and $3.9 \pm 1.7$ MPa, which are in the range of interest for dielectric elastomer actuators. Substrate effects can be neglected because the PDMS film was $590 \pm 120$ nm thick, which is large compared to the NI depth of $150 \pm 50$ nm. We can also exclude geometrical artifacts because the spherical tip has a radius of $522 \pm 2$ nm, which is small with respect to the periodicity of the wrinkles corresponding to $2800 \pm 200$ nm. In addition, the map reveals that the material on the hills is significantly stiffer with respect to the one located in the valleys.

**Discussion and conclusions**

Our results show that using a vinyl-terminated PDMS prepolymer with a number average molecular weight of $800$ g/mol, one can easily bypass the use of any solvent or curing agent to fabricate nanostructured PDMS elastomer films as thin as hundreds of nanometer.

As plasma treatments do not only change the surface morphology but also influence the chemistry and the related mechanics of the surface layers, the cross-linking

---

**Table 2:** Changing the oxygen pressure $p_{\text{ox}}$ and keeping all the other parameters constant for plasma-treated $350 \pm 50$ nm PDMS films

<table>
<thead>
<tr>
<th>Oxygen pressure $p_{\text{ox}}$, Pa</th>
<th>Contact angle $\theta$, deg</th>
<th>Hysteresis $\Delta \theta$ at $\alpha = 90^\circ$, deg</th>
<th>Periodicity of the wrinkles $\lambda$, nm</th>
<th>Amplitude $A$, nm</th>
</tr>
</thead>
<tbody>
<tr>
<td>18</td>
<td>96 $\pm$ 1</td>
<td>10 $\pm$ 1</td>
<td>1800 $\pm$ 200</td>
<td>$-80$</td>
</tr>
<tr>
<td>30</td>
<td>98 $\pm$ 1</td>
<td>10 $\pm$ 1</td>
<td>1600 $\pm$ 150</td>
<td>$-70$</td>
</tr>
<tr>
<td>35</td>
<td>96 $\pm$ 1</td>
<td>10 $\pm$ 1</td>
<td>1300 $\pm$ 150</td>
<td>$-30$</td>
</tr>
<tr>
<td>45</td>
<td>105 $\pm$ 1</td>
<td>10 $\pm$ 1</td>
<td>1100 $\pm$ 100</td>
<td>$-25$</td>
</tr>
</tbody>
</table>
mechanism via reactive species generated through photoinization and ion bombardments have to be considered. As previously shown, the irradiation of PDMS with light at wavelengths of approximately 170 nm leads to scissions of the Si-CH$_3$ and Si-CH$_2$-H bonds. The resulting unsaturated bonds give rise to a three-dimensional elastomer network (33, 35). It should be noted that we observed a strong adherence of the PDMS films to the Si wafer. It cannot be removed simply by wiping or by washing out in ethyl acetate. This effect could be associated with the comparably low wrinkle periodicity of the thinner films because the plasma treatment also affects layers well below the surface.

The wrinkling phenomena of a simple bilayer system are understood (36). It has been shown that a compressed film on a much less stiff elastomer undergoes wrinkling to relieve the intrinsic compressive stress. The orientation of the wrinkles is generally random. Buckling models can precisely predict the periodicity of these randomly oriented wrinkles $\lambda$ (21):

$$\lambda = 2\pi h_s \left( \frac{(1-\nu_s^2)E_s}{3(1-\nu_s^2)E_f} \right)^{1/3},$$  

where $h_s$ corresponds to the thickness of the stiffer film, $E_s$ and $\nu_s$ are the elastic moduli and the Poisson’s ratios of the two components, respectively. This two-layer model, however, does only partially account for the plasma-treated PDMS. The plasma treatment does not only produce a nanometer-thin film of increasing thickness but probably also changes the elastic properties of the underlying elastomer. Assuming that unchanged plasma treatment conditions result in alike parameters.
$h_i$ and $E_i$, and the thinner films are more intensely plasma-treated resulting in an increased $E_s$, according to Equation (1), the ratio $E_s/E_i$ becomes smaller, giving rise to a shorter periodicity. We have observed such a behavior, as listed in Table 1 and represented in Figure 5. The periodicity $\lambda$ decreases with the decrement in film thickness. The amplitude $A$ of the wrinkling pattern is proportional to the square root of the buckling strain $\varepsilon$ (36). Neglecting the impact of the Poisson coefficients, one finds

$$\varepsilon = \left(\frac{9E_s^2}{64E_i}\right)^{1/3}.$$  

As the treatment duration $t_{\text{plasma}}$ could influence the bulk elastic modulus $E_s$, the model correlates well with our findings. For $t_{\text{plasma}} = 144$ s, we have demonstrated a 10-fold amplitude increase. According to Equation (1), one should observe a periodicity decrease. Instead, the experiments show a constant value. Here, we speculate that the thickness $h_i$ is increasing with treatment duration. Reducing the oxygen pressure $p_{\text{ox}}$ as given by the data in Table 2 and Figure 6, one can reasonably assume that $E_s$ increases. Therefore, both the amplitude $A$ and the periodicity $\lambda$ are similarly influenced, as described by means of Equations (1) and (2).

The mechanical properties of a plasma-treated PDMS film locally measured with submicrometer precision reveals that the elastic modulus of the material in valleys differs from that on hills. The difference by a factor of two is surprisingly high. So far, one can only speculate on the reasons. We know the cross-sectional profiles of wrinkle’s networks. Geometrical phenomena related to the sinusoidal microstructure could be a reason but probably do not explain such a large effect. We further know that the wrinkle formation is associated with significant material transport (37). Therefore, one can reasonably assume a thickness modulation of the silicate layer according to the wrinkle structure.

The wetting of the aged, nanostructured PDMS films, as studied by contact angle goniometry, was improved for the ones with smaller amplitude and wrinkle periodicity. Smaller contact angles are also found on samples treated at lower oxygen pressures. This could be due to the higher SiO$_x$ concentration on the surface exposed to increased number of ion bombardments at lower oxygen pressures $p_{\text{ox}}$. The hysteresis $\Delta\theta$ at $\alpha = 90^\circ$ is found to be constant for all samples showing a value of $10^\circ \pm 1^\circ$. All samples were stored under ambient conditions for a period of 180 days. The contact angle of water on a surface plasma-treated with $P_{\text{plasma}} = 200$ W, $t_{\text{plasma}} = 18$ s, $T_s = 20^\circ C$ and $p_{\text{ox}} = 45$ Pa corresponded $49^\circ \pm 1^\circ$ several hours after fabrication and increased to $77^\circ \pm 1^\circ$ and $85^\circ \pm 1^\circ$ after 2 and 3 weeks, respectively. It is worth mentioning that plasma-polymerized PDMS films recover similarly to plasma-treated cross-linked PDMS films. Further investigations are required to analyze the prospects and challenges of these wrinkled elastomer films to serve as a support for stretchable electrodes and their integration in the field of artificial muscles and medical implants.

**Acknowledgments:** The financial support of the nanoteca.ch initiative (grant/award no. “SmartSphincter RTD2013”), project SmartSphincter, as well as the Swiss Nanoscience Institute (SNI) for the financial contribution to the AFM is gratefully acknowledged. The authors also
thank Dr. Thomas Pfohl and Dr. Tino Töpper for the discussion of the results presented.

Conflict of interest statement: Authors state no conflict of interest. All authors have read the journal’s publication ethics and publication malpractice statement available at the journal’s website and hereby confirm that they comply with all its parts applicable to the present scientific work.

References


Bionotes

Bekim Osmani
Department of Biomedical Engineering, Biomaterials Science Center, University of Basel, Gewerbestrasse 14, 4123 Allschwil, Switzerland
bekim.osmani@unibas.ch

Bekim Osmani is a PhD student at the Biomaterials Science Center at the University of Basel. He did his BSc in Mechanical Engineering and his MSc in Biomedical Engineering and Robotics at the Swiss Federal Institute of Technology in Zurich (ETHZ) in 2002. After several years of experience in academia and industry, he is currently working toward his PhD degree in nanosciences. His research interests include molecular beam deposition and electrospraying of nanometer thin elastomer films, atomic force microscopy, nanoindentation techniques and mechanical properties of nanometer thin film, polymeric implants and biomedical applications for low-voltage dielectric elastomer actuators.

Gabriela Gerganova
Department of Biomedical Engineering, Biomaterials Science Center, University of Basel, Gewerbestrasse 14, 4123 Allschwil, Switzerland

Gabriela Gerganova, 22 years old, is an integrated master’s student of pharmacology at University of Glasgow. She performs her placement year at the Biomaterials Science Centre under the direction of Prof. Bert Müller. Her research focus is on the formulation, characterization and safety of liposome-based nanocontainers for targeted drug delivery. During her internship, she has expanded her practical skills in biomedical engineering with the help of on-site laboratory facilities.

Bert Müller
Department of Biomedical Engineering, Biomaterials Science Center, University of Basel, Gewerbestrasse 14, 4123 Allschwil, Switzerland

Bert Müller received a diploma in mechanical engineering, Berlin 1982, followed by MSc degrees in Physics and English both from the Dresden University of Technology in 1989. In 1994, he obtained a PhD in experimental physics from the University of Hannover, Germany. For his achievements, he was granted with the Morton M. Traum Award of the American Vacuum Society in 1994. From 1994 to 2001, he worked as a researcher at the Paderborn University, Germany, as Feodor Lynen Fellow and research associate at the EPF Lausanne, Switzerland and as team leader at the Physics Department, Materials Department and Department of Information Technology and Electrical Engineering at ETH Zurich, Switzerland. He became a faculty member of the Physics Department at ETH Zurich in April 2001. After his election as Thomas Straumann-Chair for Materials Science in Medicine at the University of Basel, Switzerland and his appointment at the Surgery Department of the University Hospital Basel in September 2006, he founded the Biomaterials Science Center in March 2007. Currently, this center hosts more than 20 researchers dealing with nanotechnology-based artificial muscles for incontinence treatment, smart nanocontainers to treat cardiovascular diseases, high-resolution X-ray imaging to visualize the human body down to the molecular level, computational sciences of tissues in health and disease and other applications of nanosciences in medicine. The mission of the research team can be summarized by using physical principles for human health. Professor Müller teaches physics and materials science at the ETH Zurich and the University of Basel and currently supervises doctoral students from medicine, dentistry, physics, nanosciences and biomedical engineering. He was elected as Fellow of SPIE in 2014 and as an active member of the European Academy of Sciences and Arts in 2015.